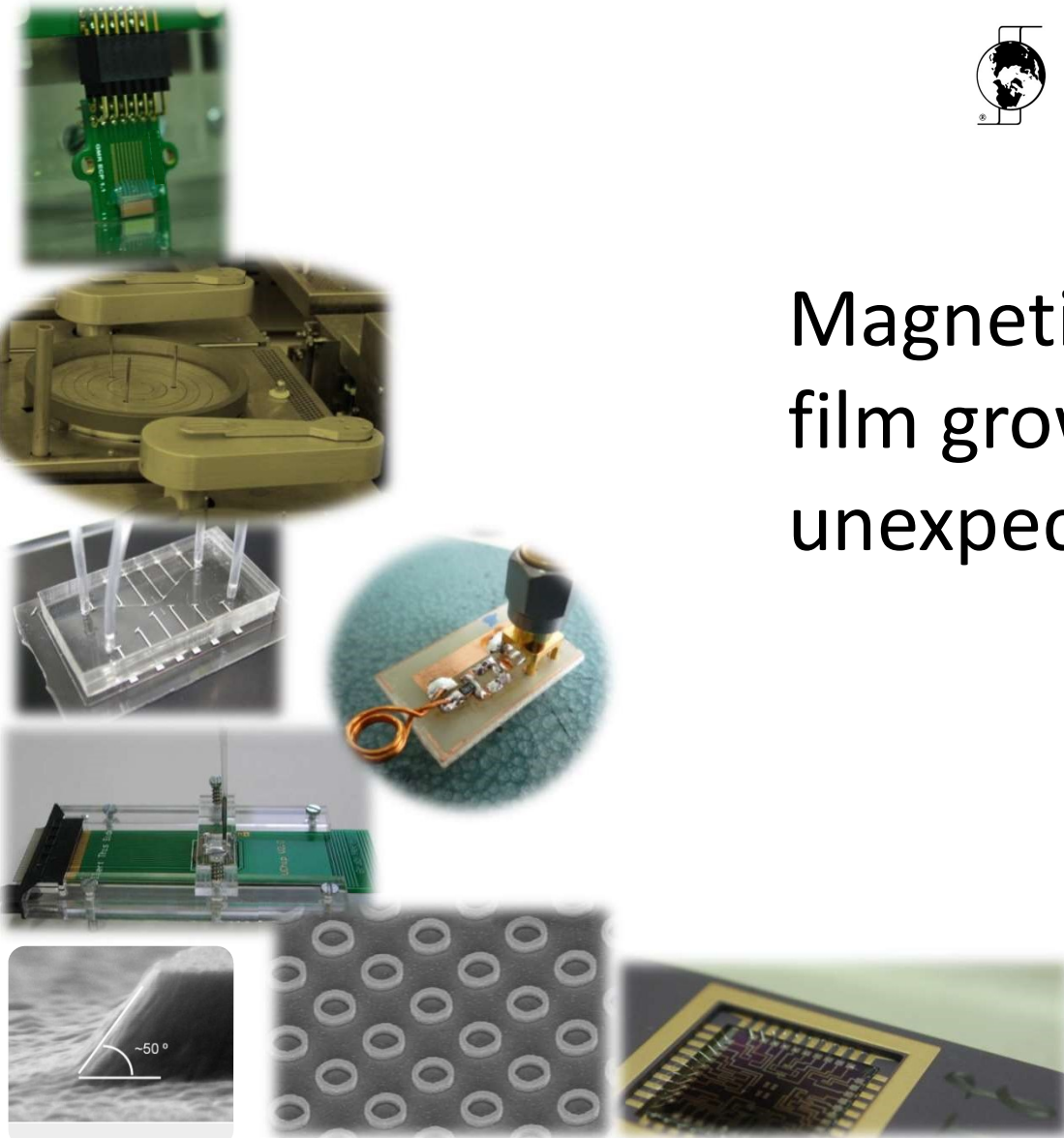


Magnetic sensors: from ultrathin film growth to sensor integration in unexpected systems

Susana Cardoso de Freitas

Group leader Spintronics & Magnetic Sensors

INESC – Microsystems and Nanotechnologies
Lisbon, Portugal
www.inesc-mn.pt



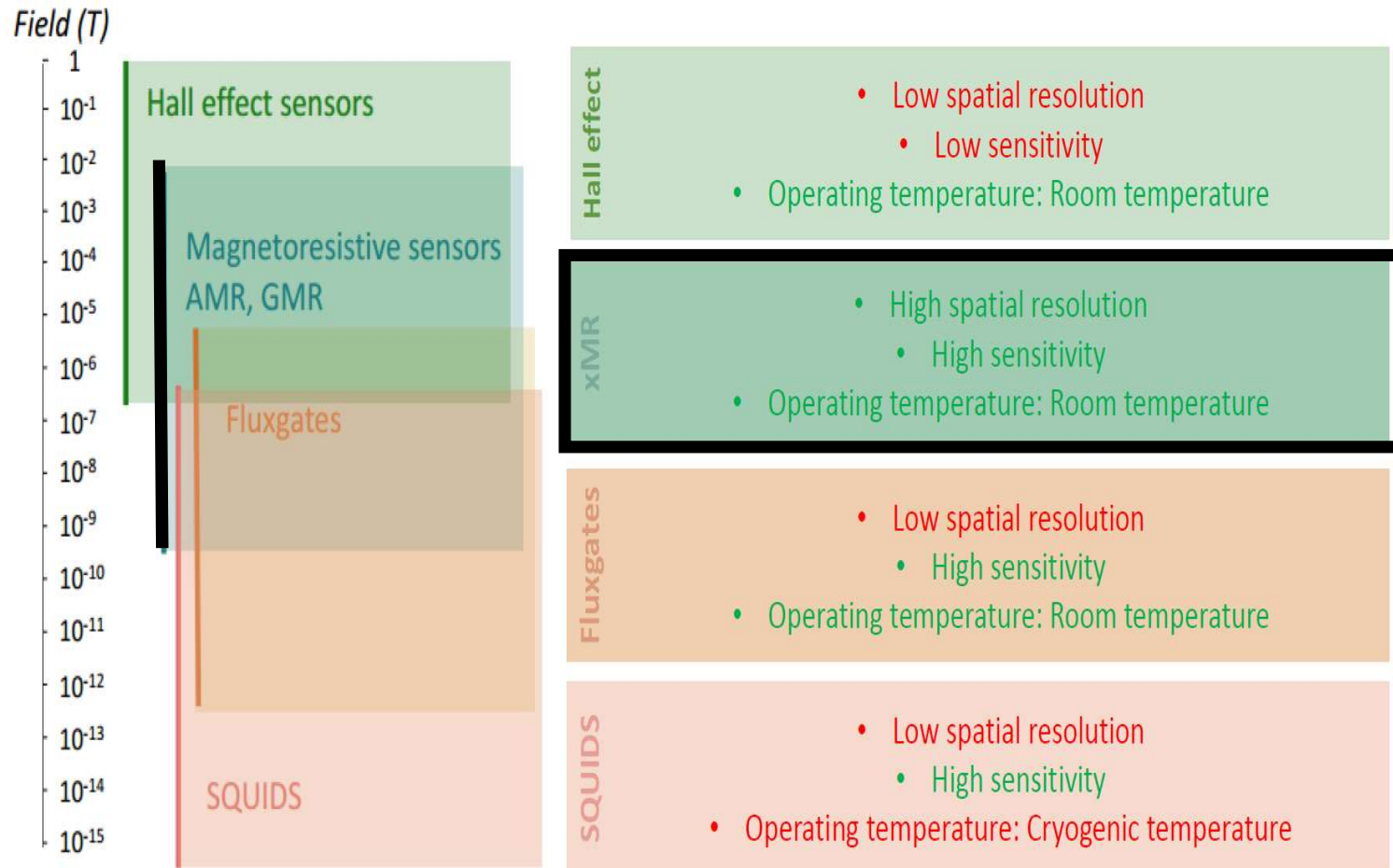
Outline

Magnetoresistive sensors

- thin film materials
- thermal stability
- noise, SNR => detectivity for pT
- 3D detection on chip

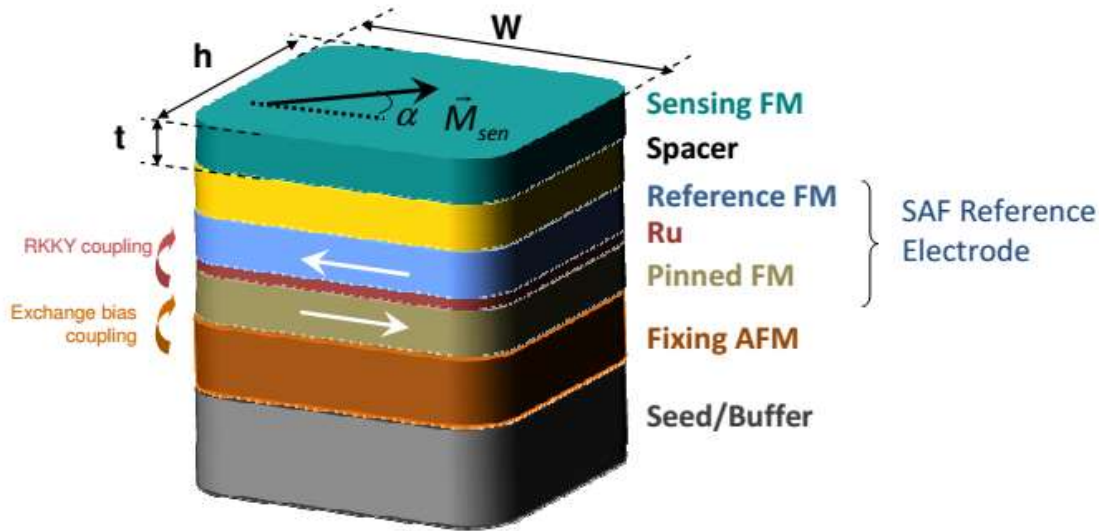
Applications

Magnetic sensors



xMR sensors

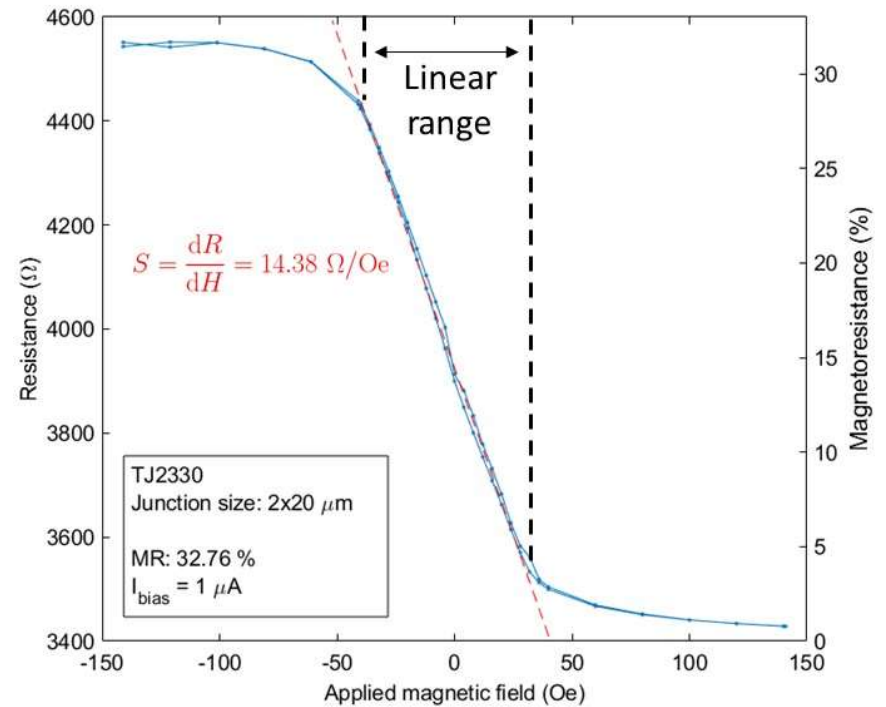
WHY MAGNETORESISTIVE SENSORS ARE CANDIDATES FOR MANY APPLICATIONS ?



Magnetoresistance

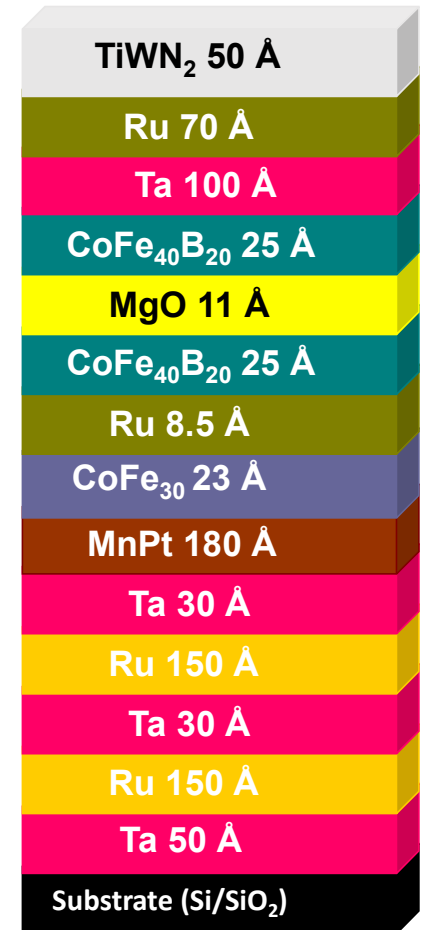
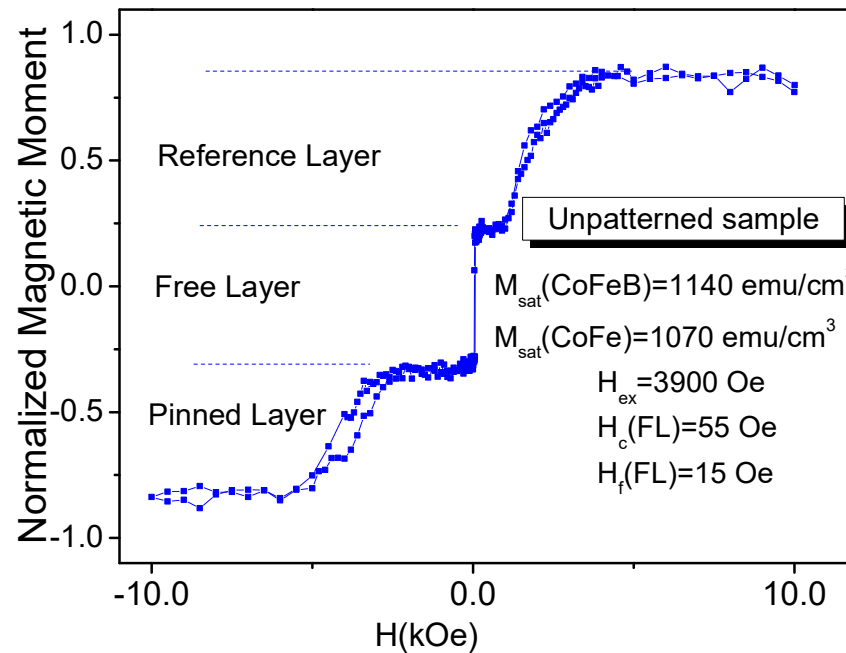
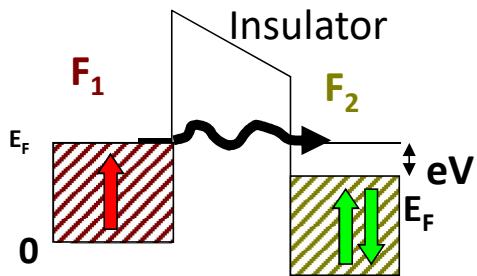
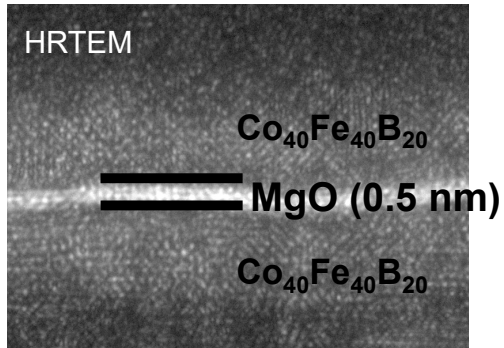
$$MR = \frac{R_{max} - R_{min}}{R_{min}}$$

AMR: 2-5%
GMR: 6~15%
Al₂O₃ TMR: 20~40%
MgO TMR: 80~260%



Linear range
 $\Delta H \sim 10\text{-}300$ Oe
(1-30 mTesla)

Magnetic tunnel junction - TMR

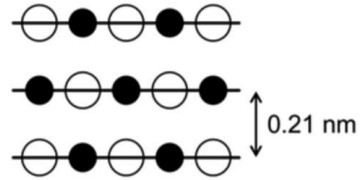
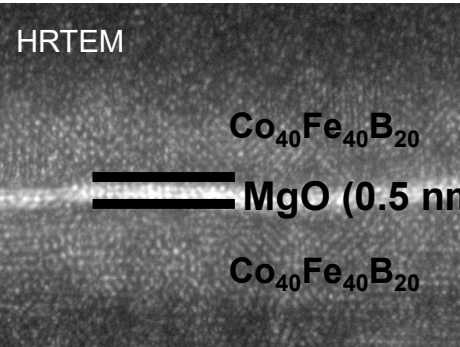


MIT, 1996
IBM, 1997
INESC, 1997

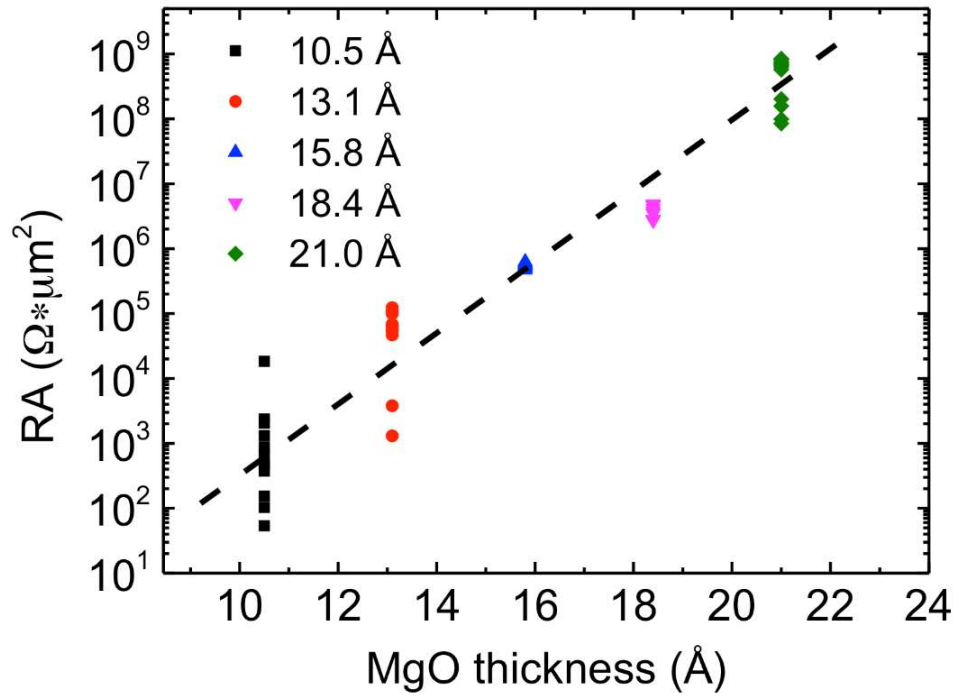
Electrons will tunnel if apply voltage between electrodes
Spin is conserved upon tunneling

Accurate control of the thin film thickness

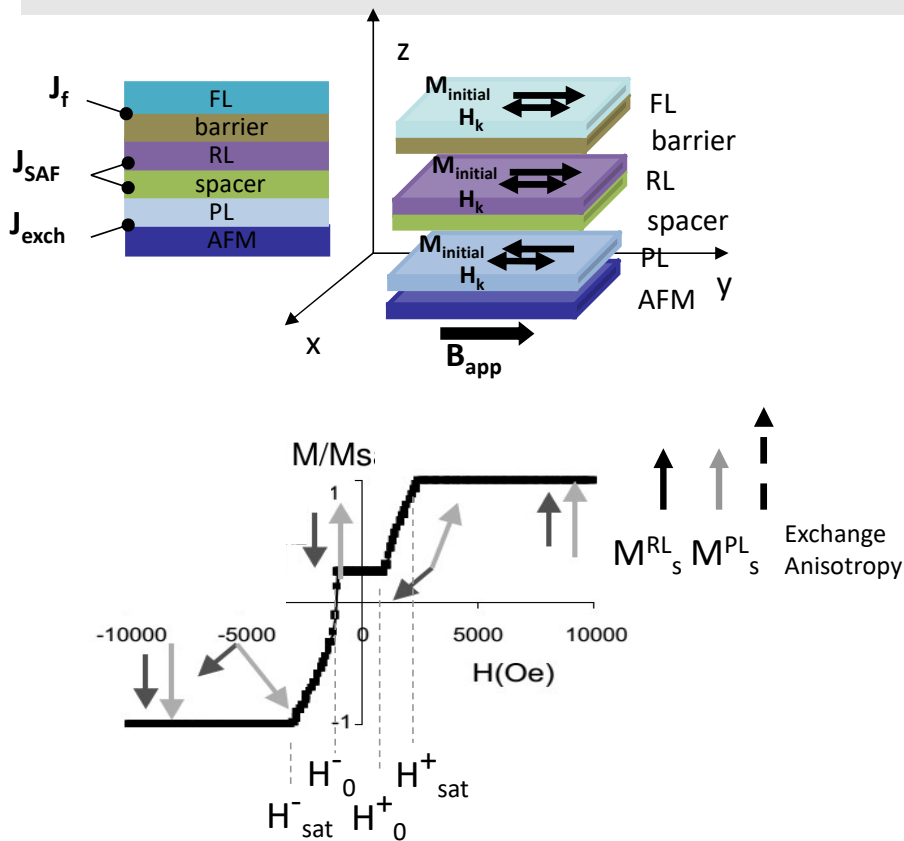
- impact on TMR
- impact on R



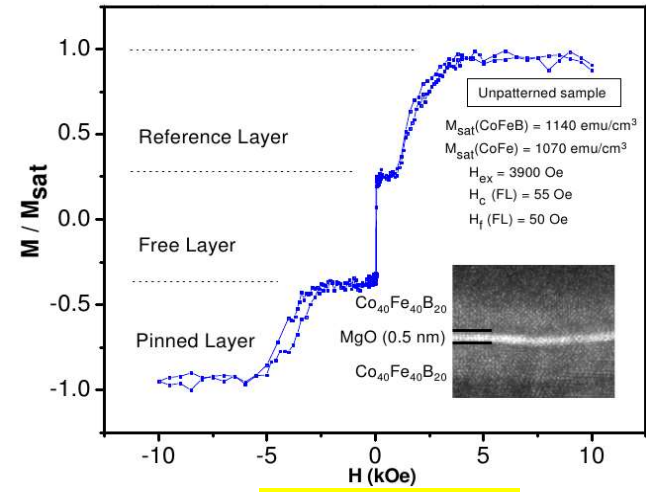
1 Å => 10x R



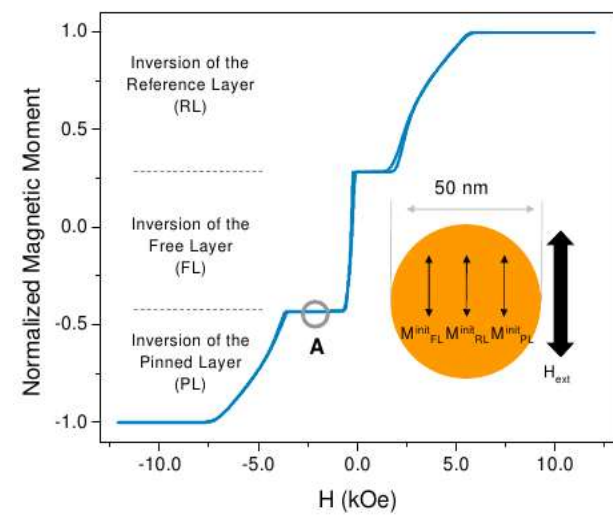
Micromagnetic and Analytical Models



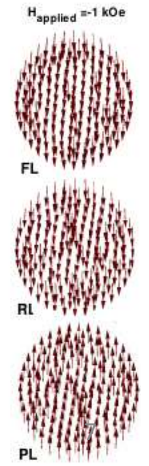
Experimental



Simulation

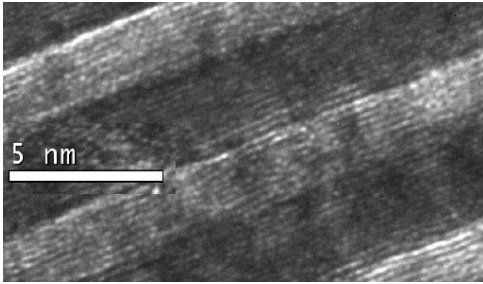


Micromagnetic distributions at A



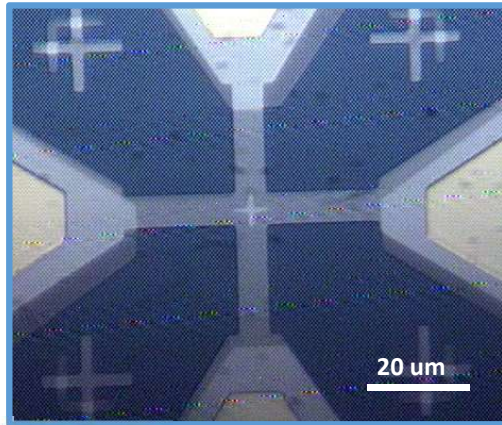
Magnetolectronics, Elsevier, Ed. Mark Jonhson, 2004
 IEEE Trans.Magn.49 (7), pp. 4405-4408 (2013)
 Nanotechnology 27, 045501 (2015)
 Physica B: Cond. Matter, 435, 163 (2014)

Scientific Reports , 11, 215 (2021)
 Appl.Phys.Letters 118, 072401 (2021);
 Adv. Electronic Materials, 7 , 2000976 (2020)
 IEEE Magn.Mat. (in press, 2023)



Film thickness:
Controlled at the atomic scale
 $1 \text{ \AA} = 0.1 \text{ nm}$

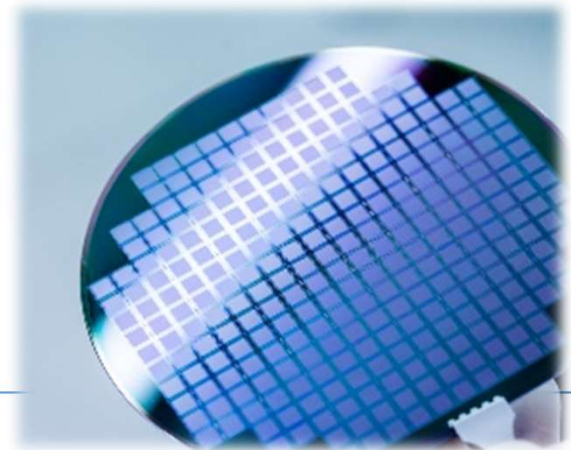
Multilevel device
patterning



MgO target with Ar plasma



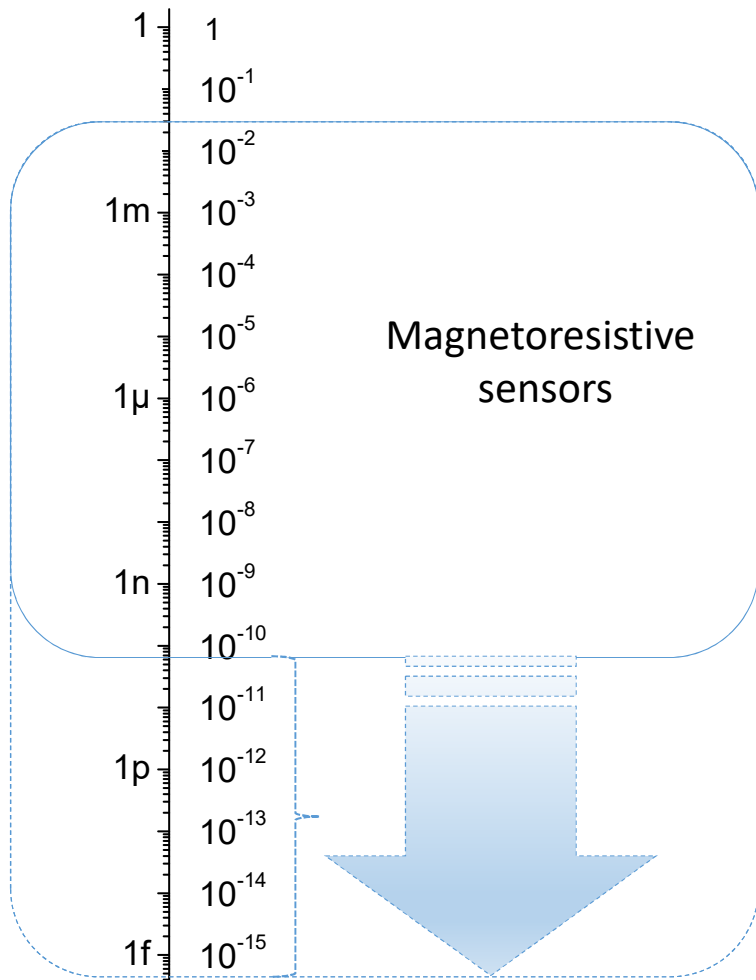
Wafer microfabrication
in a Clean Room



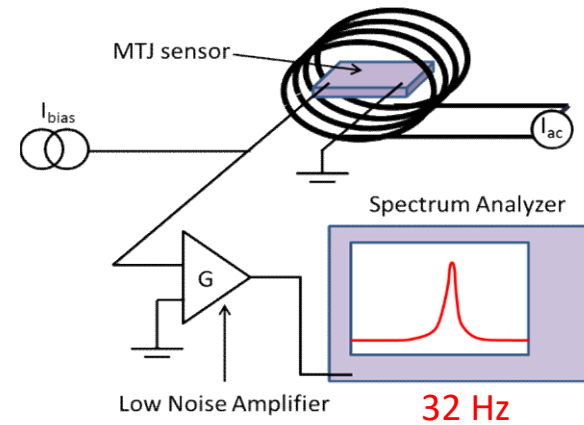
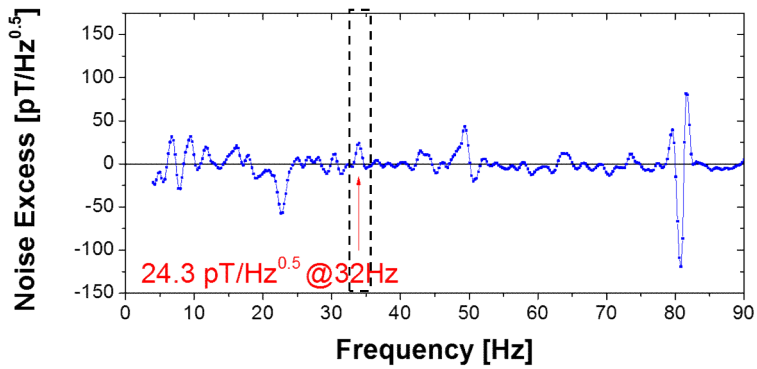
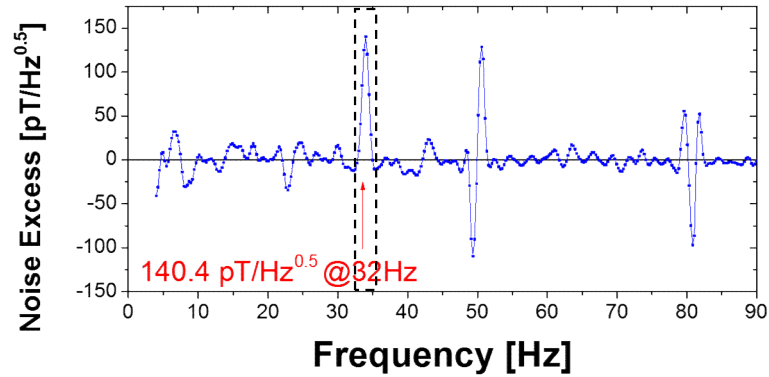
Challenges II

Low noise, high signal

Magnetic Field (Tesla)



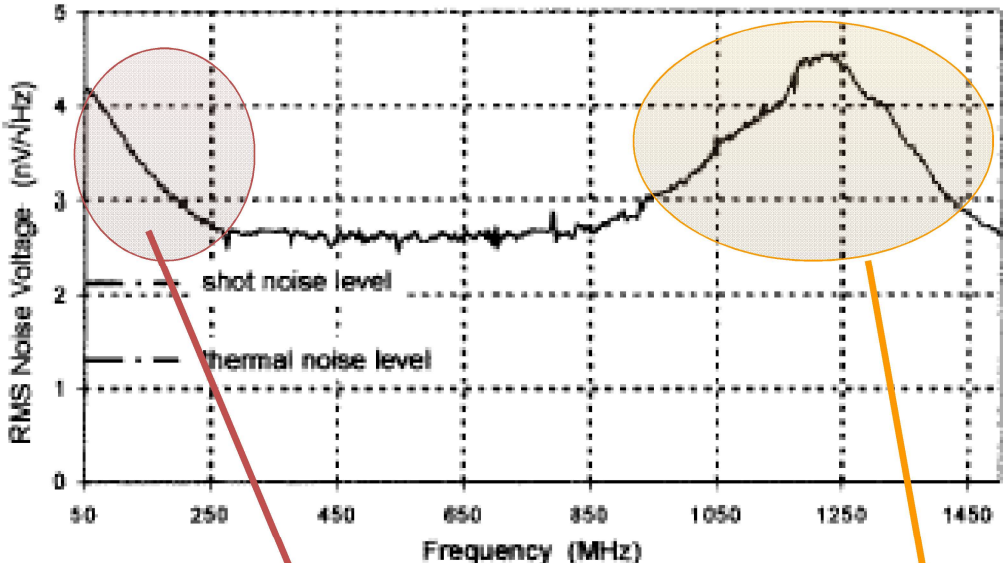
How to distinguish signal from noise ?



Detectivity limit:
SNR = 1
 (Signal = Noise)

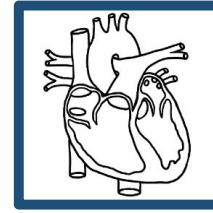
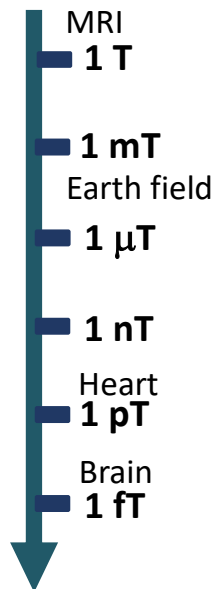
Noise Spectrum of Magnetoresistive Sensors

Main noise contributions



$$S_V (V^2 / Hz) = \frac{\alpha_H I^2 R^2}{A f \Delta f} + \frac{4K_B TR}{\Delta f} + \frac{2eIR^2}{\Delta f} + FMR_{Noise}$$

1/f noise Thermal Noise Shot Noise High-Frequency Noise



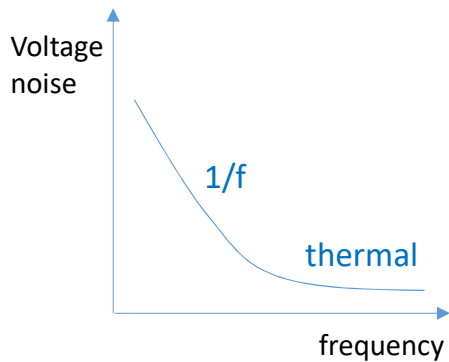
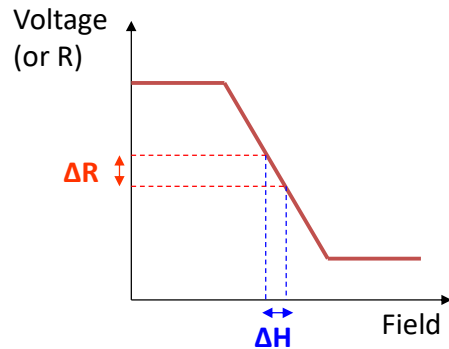
Amplitude:
few **pTesla** at chest surface
(below 100 Hz)



Amplitude:
few **fTesla** at skull surface
(below 100 Hz)

Field detectivity (D)

Detectivity limit: **SNR = 1** (Signal = Noise)



$$S_V \left(T / \sqrt{Hz} \right) = \frac{\sqrt{\frac{\alpha_H I^2 R^2}{V f}}}{I \cdot \frac{\Delta R}{\Delta H}} = \frac{\Delta H}{MR} \sqrt{\frac{\alpha_H}{V f}} \quad [\text{in Tesla}]$$

(in 1/f regime)

- Operate at high f
- Increase MR
- Increase V
- Reduce linear range ΔH
- Reduce Hooge value

$S = TMR / \Delta H$
 sensor sensitivity

α_H = Hooge's constant
 A = MR area
 f = operating frequency

Strategies to improve the minimum detectable field

Field modulation for high frequency

Increase MR

Increase V

Reduce linear range ΔH

Reduce Hooge value

Sensors, 18(3), 790; (2018)

Micromachines, 7(5), 88 (2016)

IEEE Trans. Magn. 48 (11), pp. 4115 (2012)

Journal of SPIN, Vol.1 (1), pp 71-91 (2011)

J.Appl.Phys. 103, 07E924 (2008)

Appl. Phys. Lett. 95, 023502 (2009)

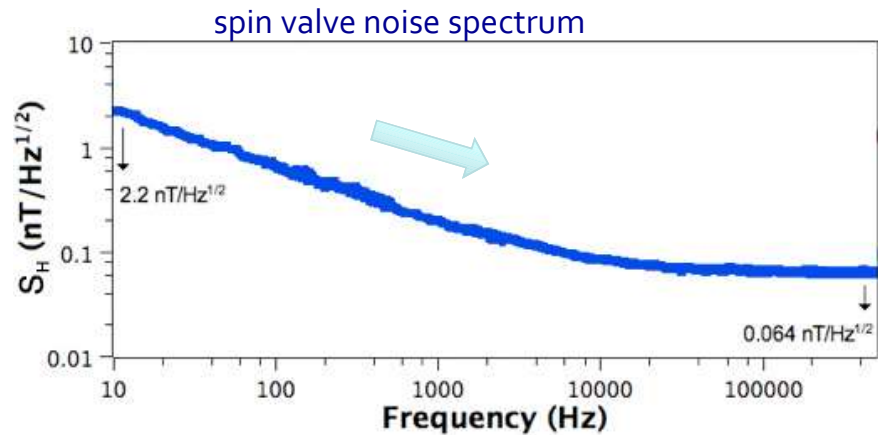
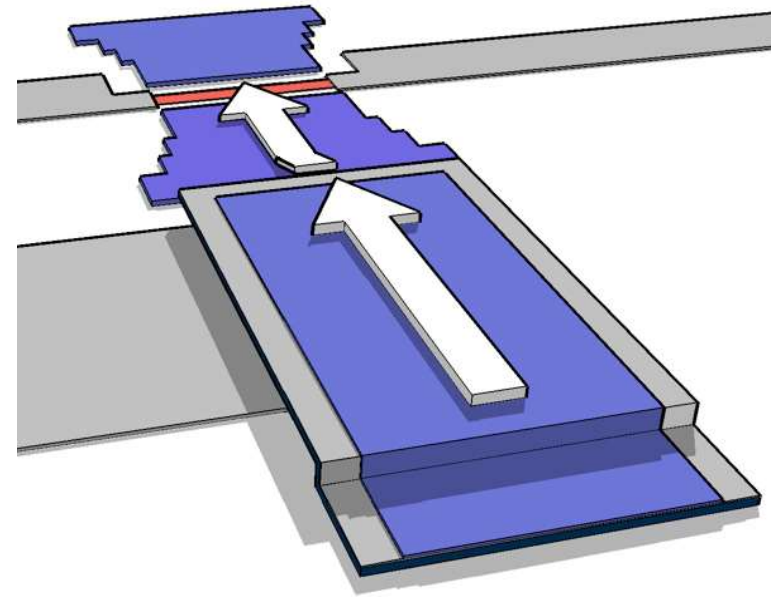
magnetic MEMS

Modulate dc magnetic field at high frequency using MEMS resonators with incorporated magnetic flux guides

goal

shift the sensor operating frequency to the kHz region where the noise can be 2 orders of magnitude lower than dc

geometry



Appl. Phys. Lett. 95, 023502 (2009)

J.Appl.Phys. 103, 07E924 (2008)

Strategies to improve the minimum detectable field

Field modulation for high frequency

Increase MR

Increase A

Reduce linear range ΔH

Reduce Hooge value

Nat Mater, 2004, 3:862–867

J PhysD-Appl Phys, 2007, 40: R337

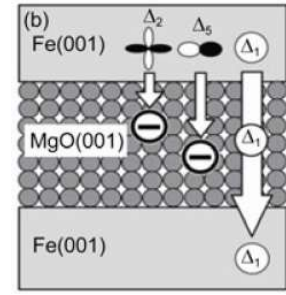
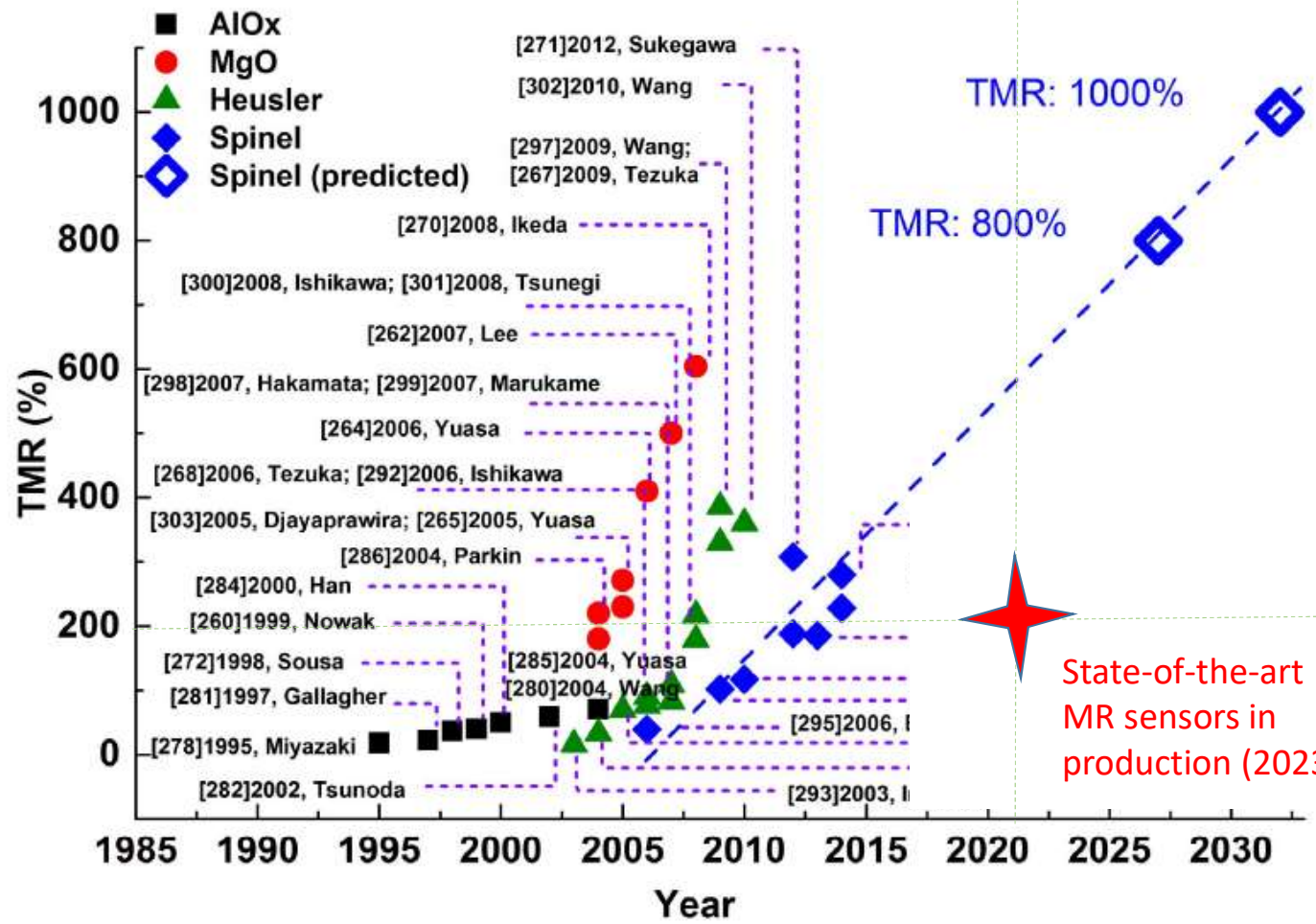
J. Physics: Cond.Matter, 19 (2007) 165221

Ann Rev Mater Res, 2009, 39: 277–296

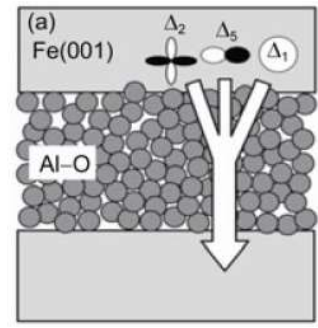
J Appl Phys, 2007, 101: 09B501

J. Appl. Phys, 99, 08A907 2006

AlOx and MgO barriers



Crystalline barrier



Amorphous barrier

"Magnetoresistive Sensor Development Roadmap (Non-Recording Applications)"
IEEE Trans.Magn. (2019)

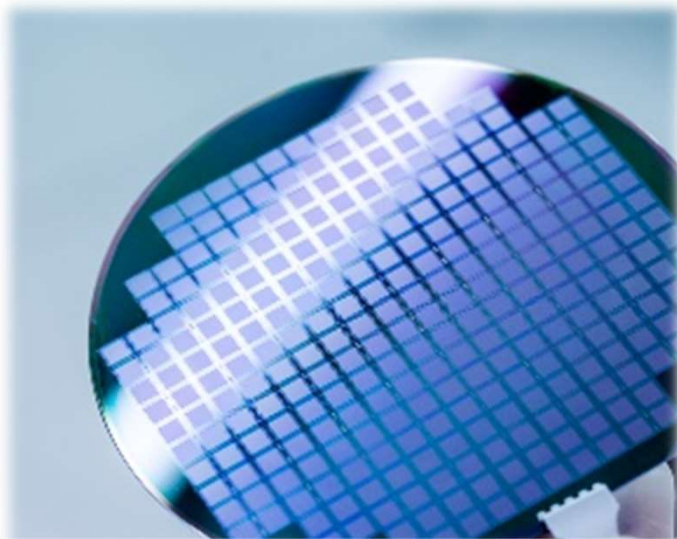
200mm backend GMR / TMR technology



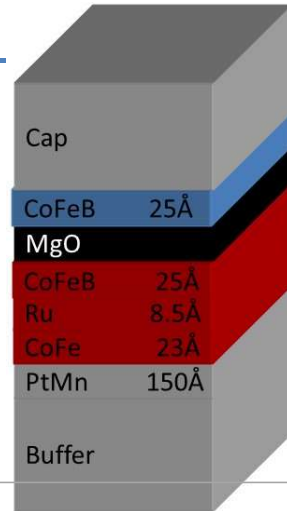
TiWN
Ta 50 A
Ru 50 A
CoFeB(t)
MgO 13.5 A
CoFeB 30 A
Ru 9 A
CoFe 22 A
IrMn 200 A
Ta 30 A
Ru 180 A
Ta 50 A
substrate

F
R
P
B

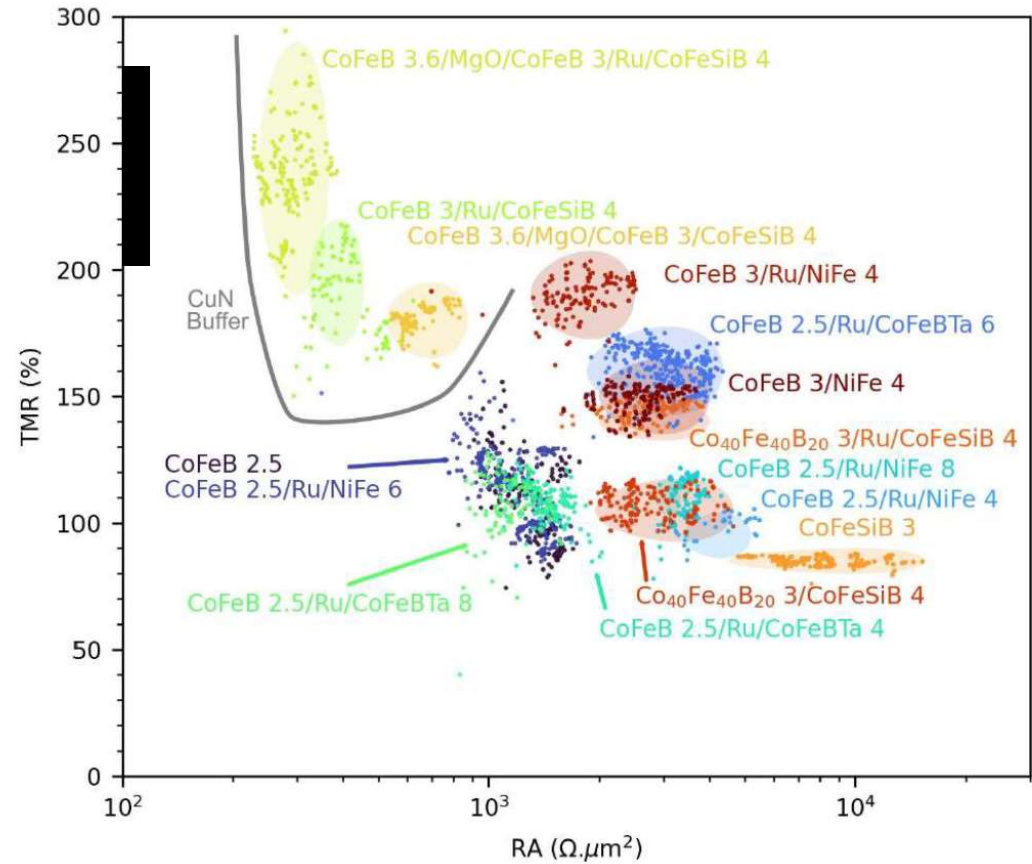
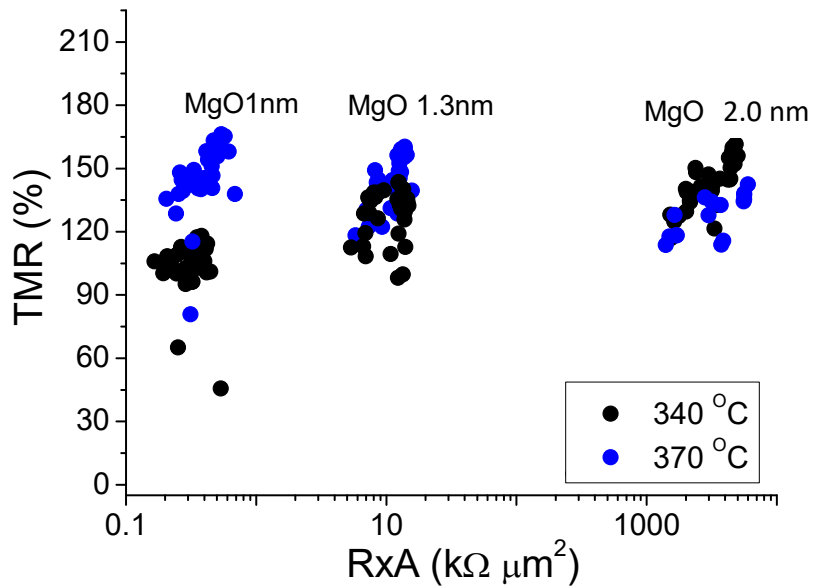
6 targets IBD (extra module
8 targets in PVD; 2019)
Dep pressure 2×10^{-5} Torr
Heated substrate
Assist gun,
Base Pressure 5×10^{-8} Torr



MgO TMR sensors



Amorphous CoFeBSi, CoFeBTa



F.Matos, et.al. **AIP-Advances**, 13, 025108 (2023);

Strategies to improve the minimum detectable field

Field modulation for high frequency

Increase TMR

Increase V (area or thickness)

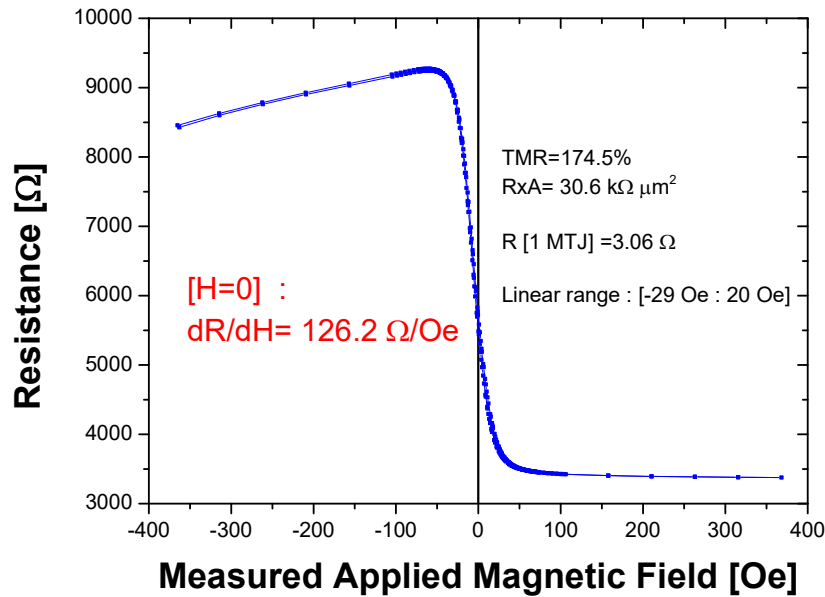
Reduce linear range ΔH

Reduce Hooge value

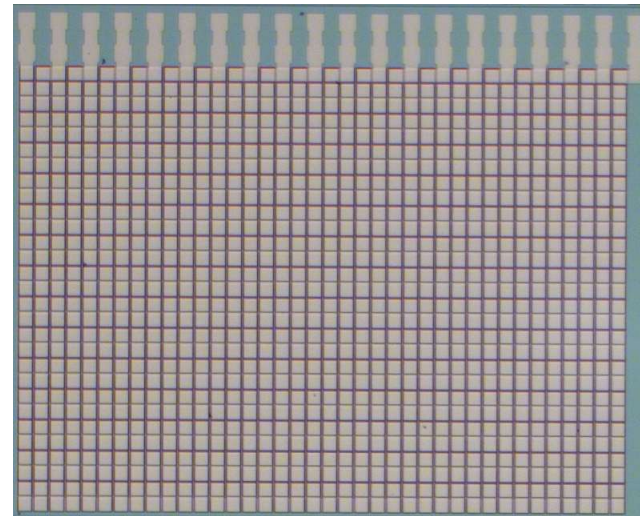
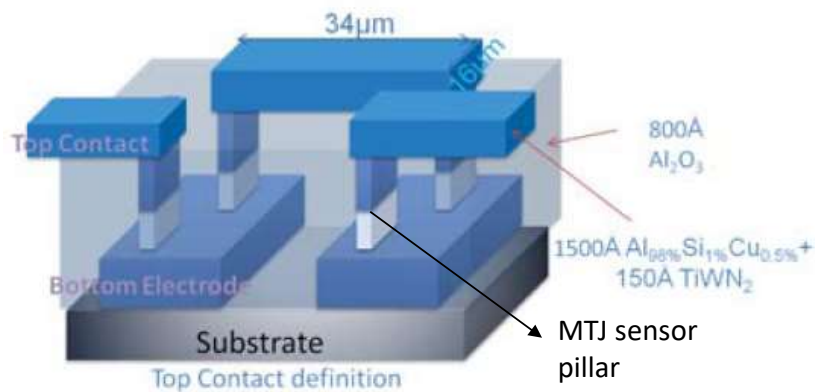
R.Chaves, et.al , Appl. Phys.Lett, 91, 102504 (2017)

E. Paz et.al – J. Applied Physics; 115. 2014

Large Series
 1102 TMR elements with
 $A = 100 \times 100 \mu\text{m}^2$ each.

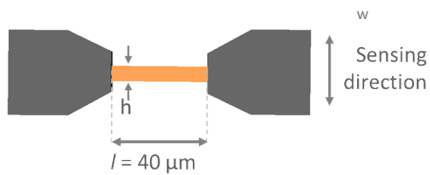


1 mm x 1 mm

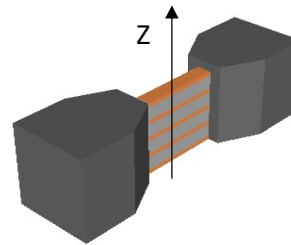


Saving space: GMR sensors packed

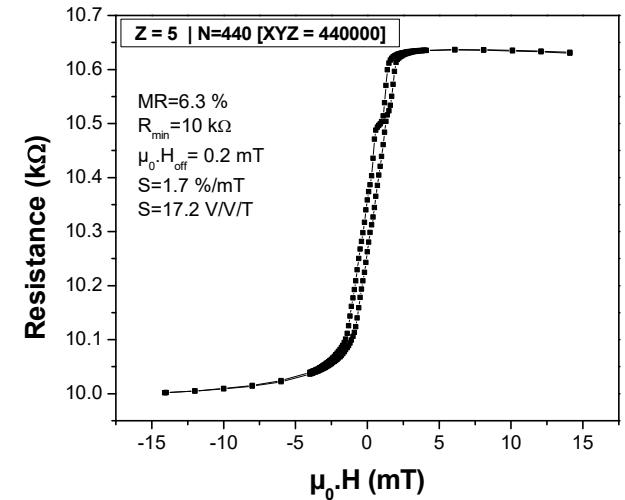
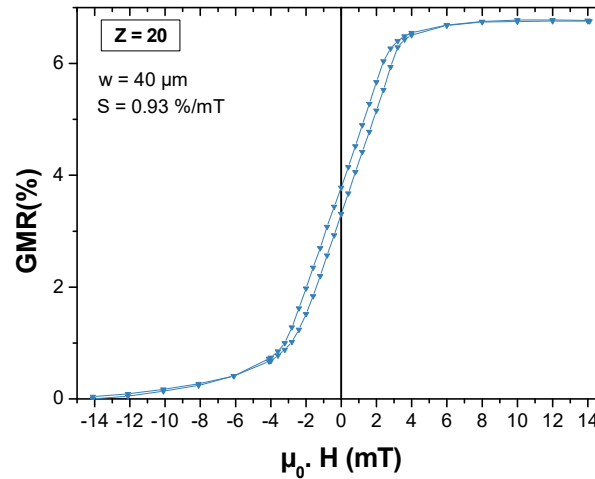
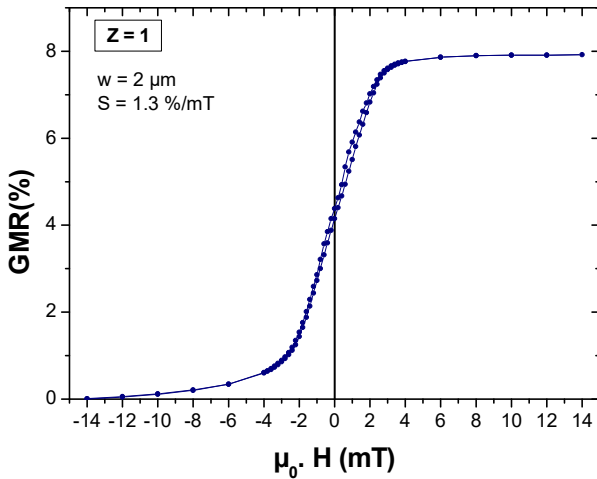
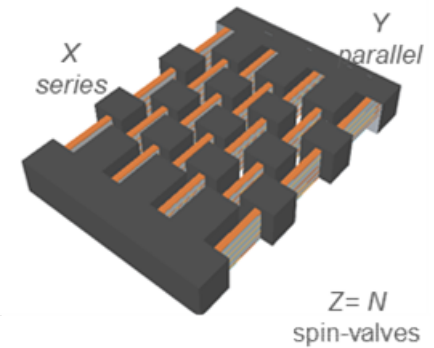
Single sensor



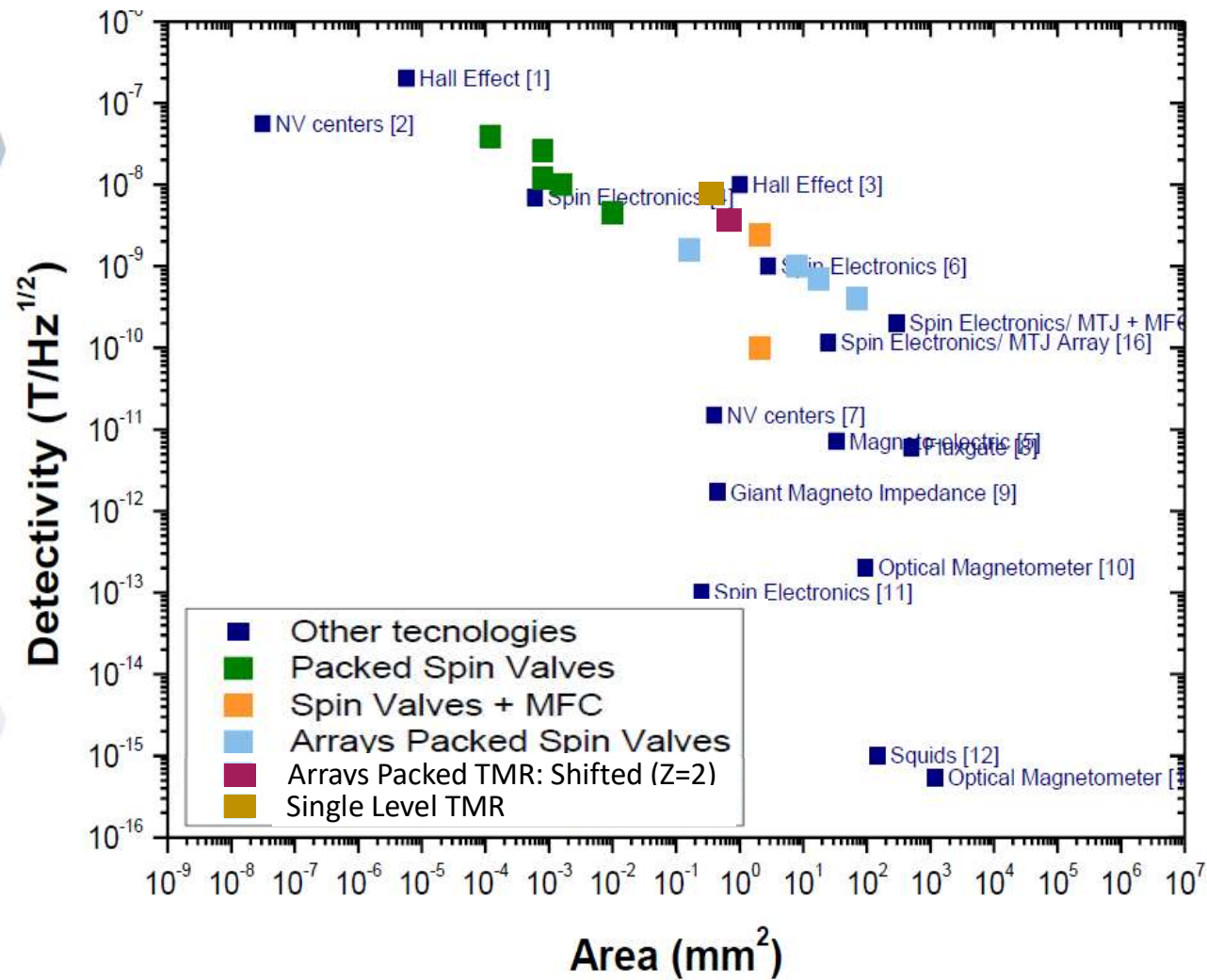
Packed sensors



Packed arrays of sensors



AIP Advances 8(5):056644 (2018)
 Scientific Reports , 11, 215 (2021)



AIP Advances 8(5):056644 (2018)
 Scientific Reports , 11, 215 (2021)

- [1] E. Paz et al., *J. Appl. Phys.*, vol. 115,2014.
- [2] tdk.com, "TDK biomagnetic sensor", 2019
- [3] S. H. Liou et al., *Proc. IEEE Sensors*, 2009

- [1] P. Besse et al *Appl. Phys. Lett.* **80**, 4199 (2002)
- [2] P. Maletinsky et al *Nature Nanotechnology* **7**, 320-324 (2012)
- [3] F. Montaigne et al *Sensors and Actuators A: Physical* **81**, 324-327 (2000)
- [4] L. Caruso et al *Neuron* **95**, 1283-1291 (2017)
- [5] R. Jahns et al *Sensors and Actuators A: Physical* **183**, 16-21 (2012)
- [6] F. Barbieri et al *Scientific Reports* **6**, 39330 (2016)
- [7] J. Barry et al *PNAS* **113**, 14133-14138 (2016)
- [8] Bartington Instruments, Mag-03 Three-axis
- [9] S. Yabukami et al *JMMM* **290**, 1318-1321 (2005)
- [10] T. Sander et al *Biomedical Optics Express* **3**, 981-990 (2012)
- [11] M. Pannetier et al *Science* **304**, 1648-1650 (2004)
- [12] J. Gallop *Supercond. Sci. Technol.* **16**, 1575 (2003)
- [13] I. Kominis et al *Nature* **422**, 596-599 (2003)
- [14] E. Paz et al., *J. Appl. Phys.*, vol. 115,2014.
- [15] tdk.com, "TDK biomagnetic sensor", 2019
- [16] S. H. Liou et al., *Proc. IEEE Sensors*, 2009

Applications

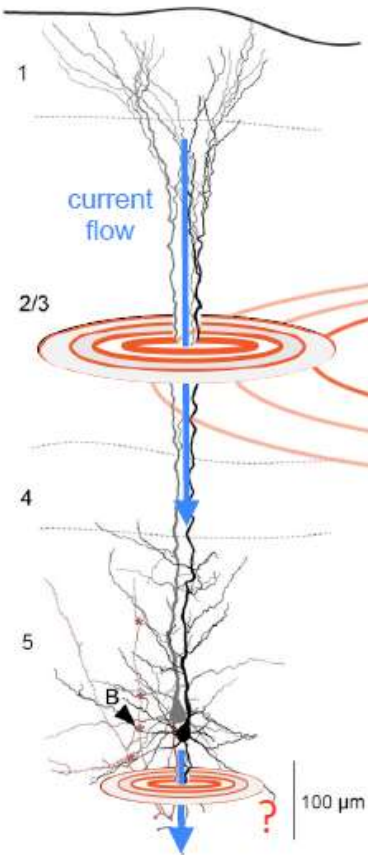
- Neurosciences
- Robotics
- Pattern readout
- Biochips



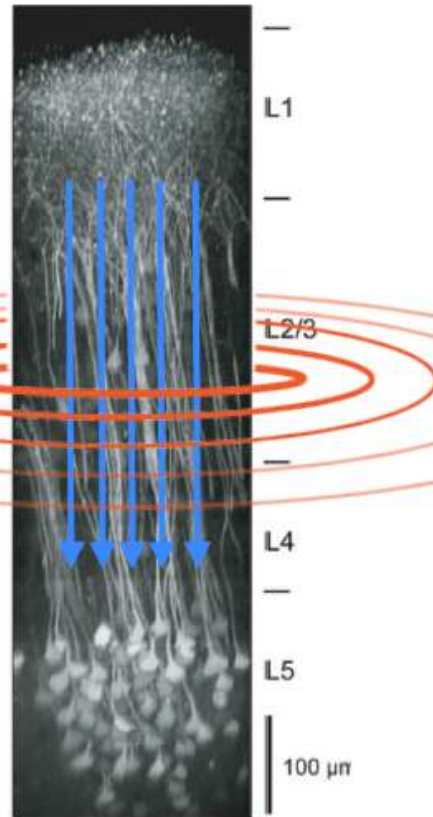
Applications

Neuronal probes with MR sensors

**Individual
 pyramidal cells**



Cell assembly



Helmchen and Denk. 2005. *Nature Methods* 2 : 932-940.

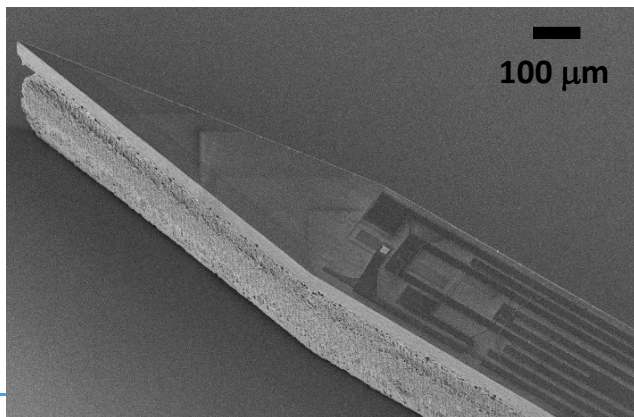
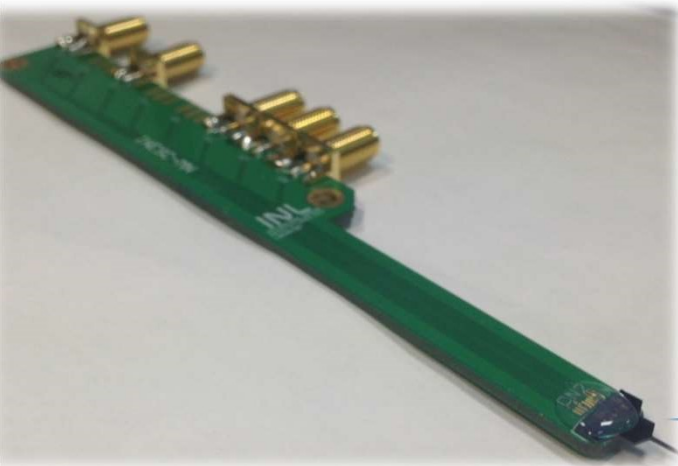
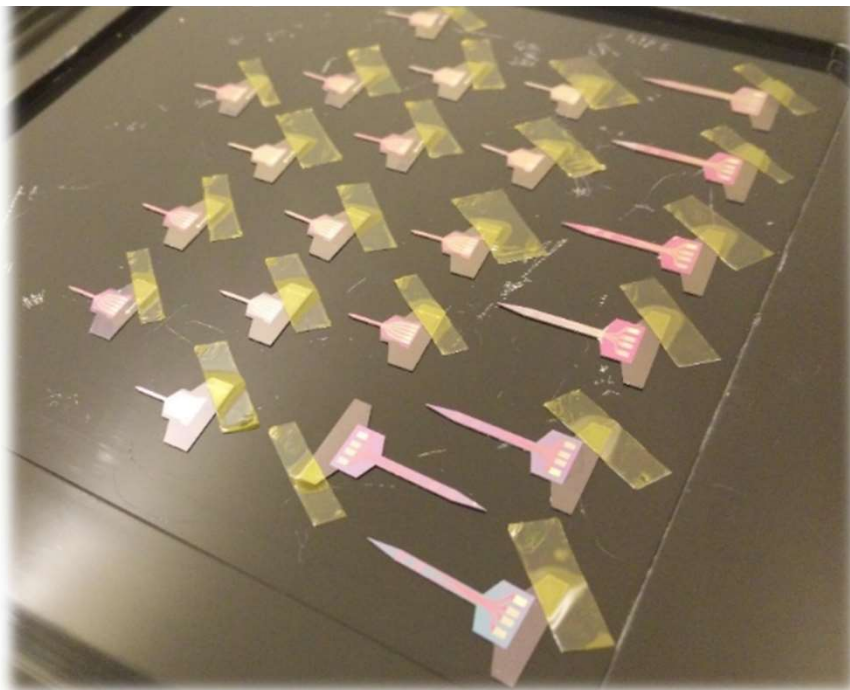
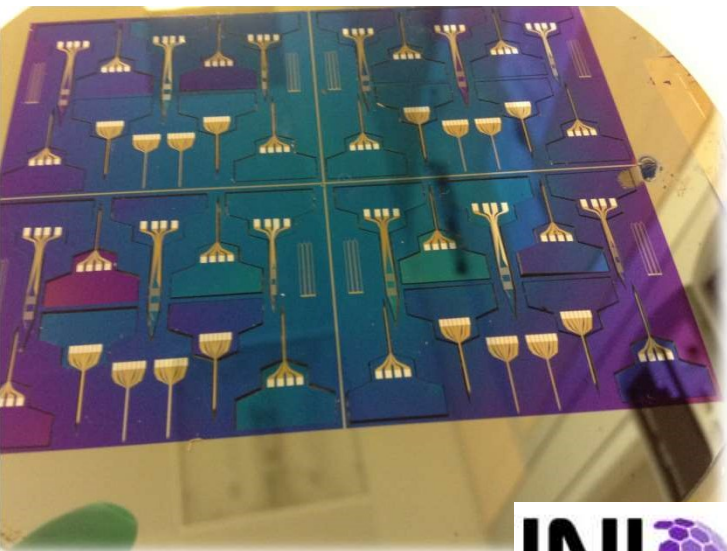
Estimation of the magnetic field:

- **MagnetoEncephaloGraphy :**
 SQUID - signal distance = 3 cm
 Field = 1 fT (Field decay : $1/(r^2)$)
- **Magnetodes:**
 MR - signal distance = 10-100 μm
 Field ≈ 100 pT – 1nT

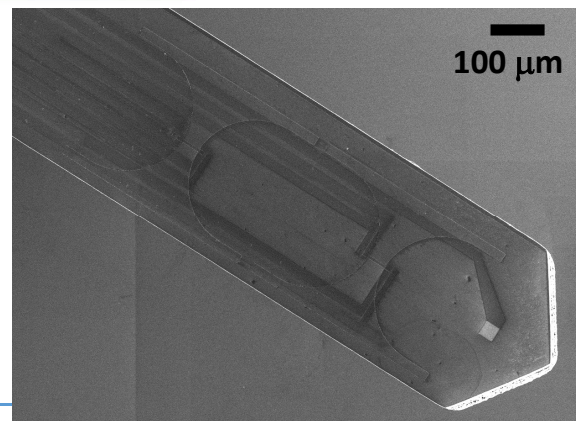
Estimated fields ~pT - nT



**FET-EU project
 Magnetodes**

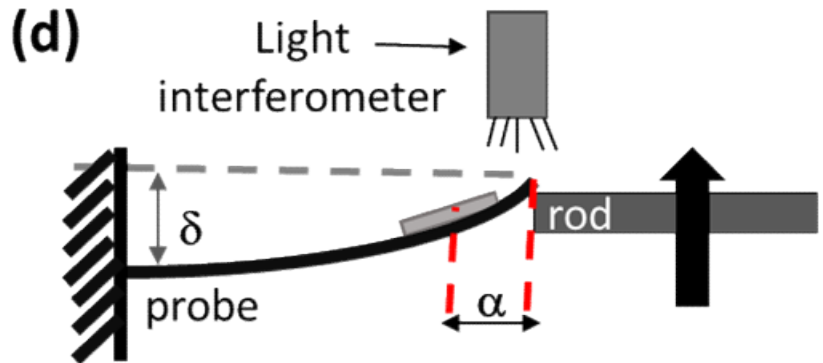
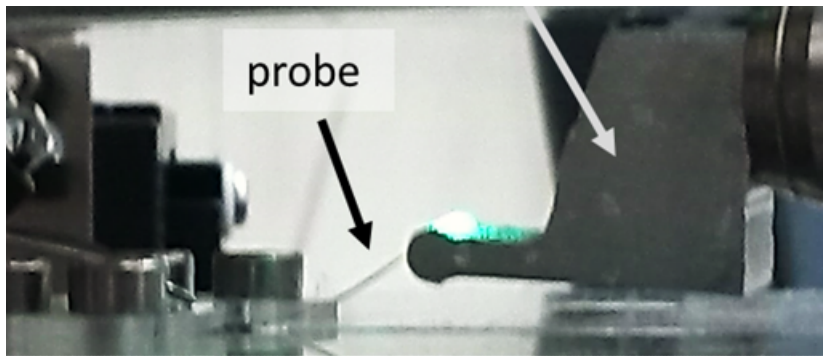


SEM image: sharp tip (*in-vivo*)



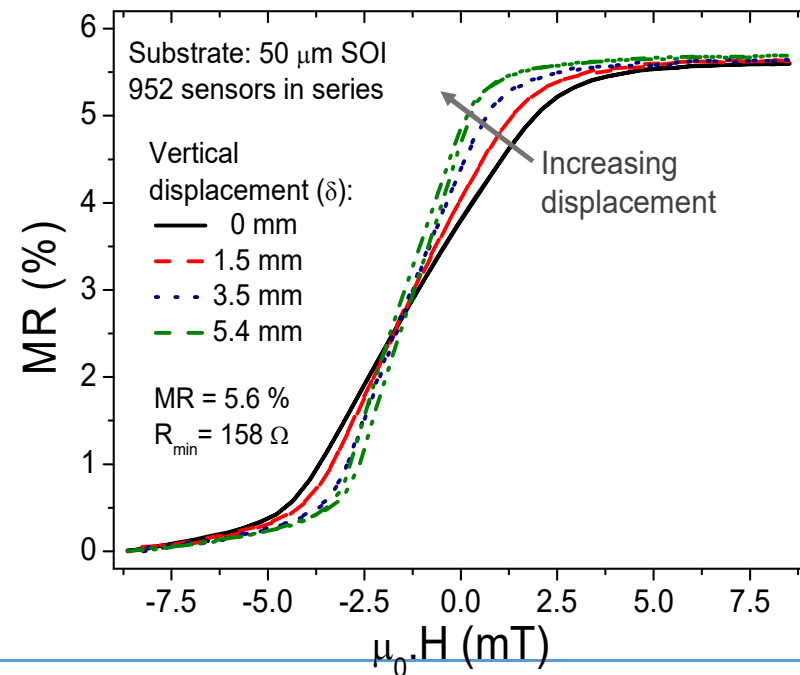
SEM image: flat tip (*in-vitro*)

When penetrating the tissues:

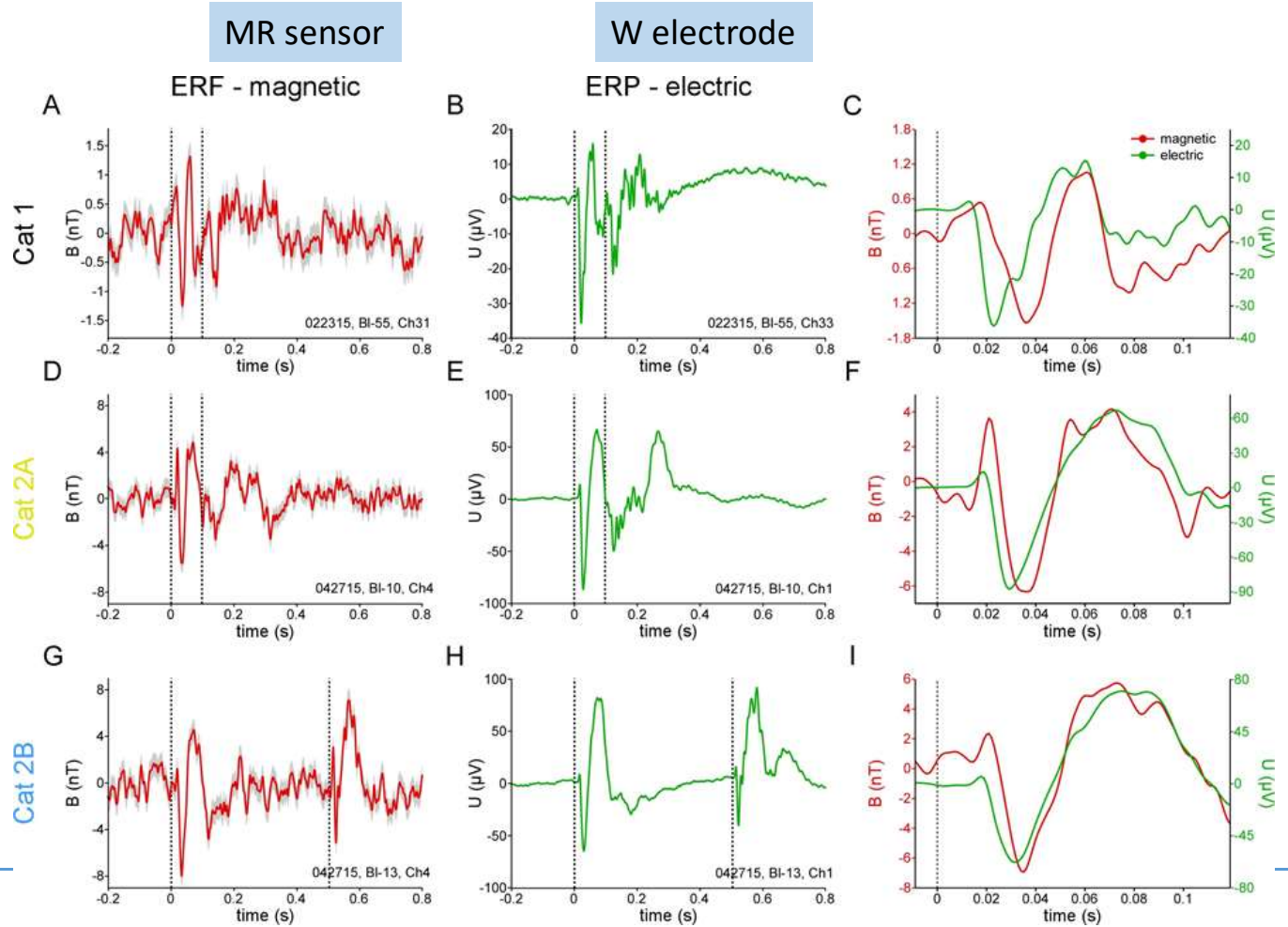
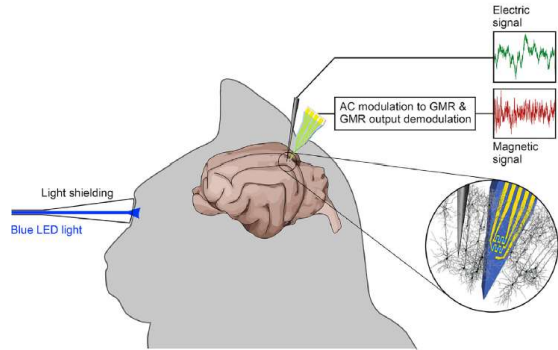


Sensor output: remains linear, non-hysteretic and without discontinuities

- axial force along the tip longitudinal direction;
- slight bending of the probe, **force perpendicular to the longest direction.**

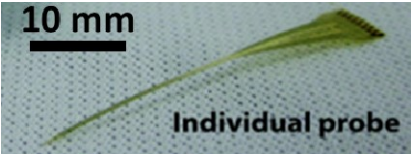
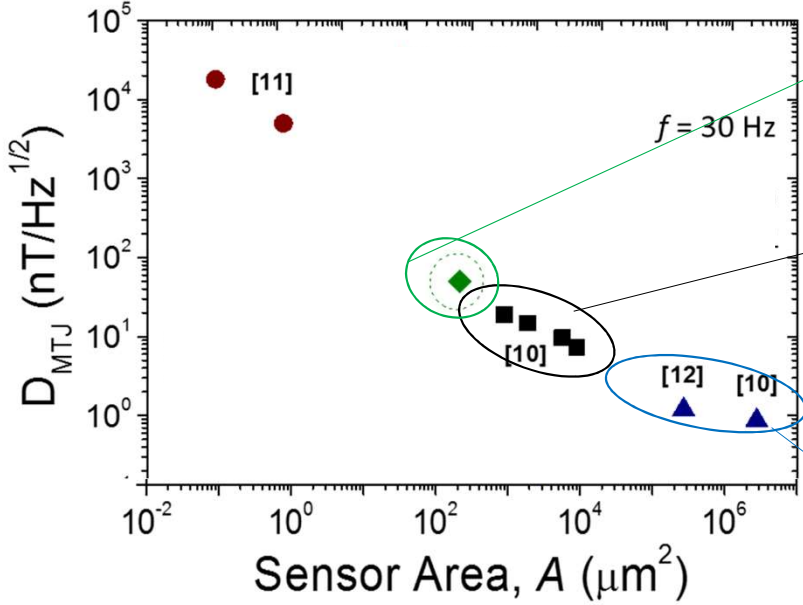


In Vivo validation of MR sensor probes

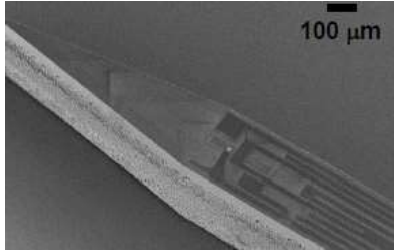


L.Caruso, S.Cardoso, P.P Freitas, P.Fries, M. Lecoer, et.al
 "In vivo magnetic recording of neuronal activity",
Neuron, 95, 1–9 (2017)

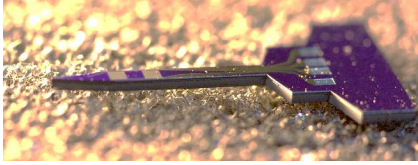
Detectivity (D) - **minimum detectable field**
 $SNR = 1$



flexible probe - polyimide



Si probe (single MR)

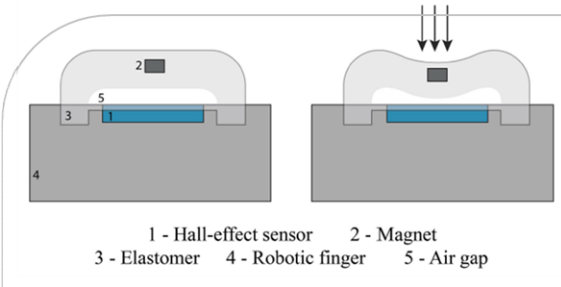
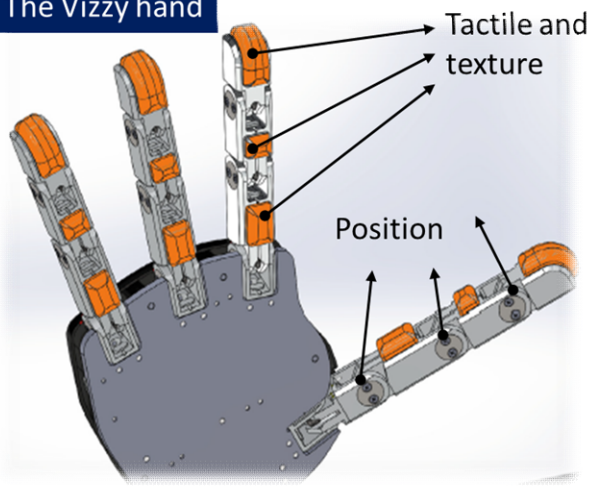


Si probe (arrays MR)

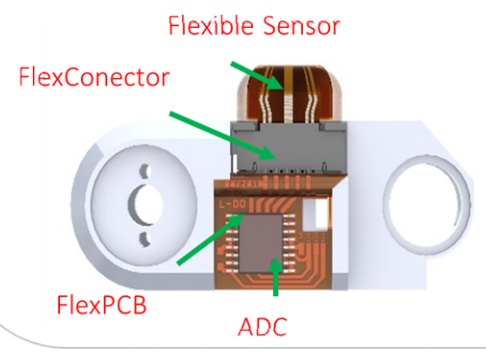
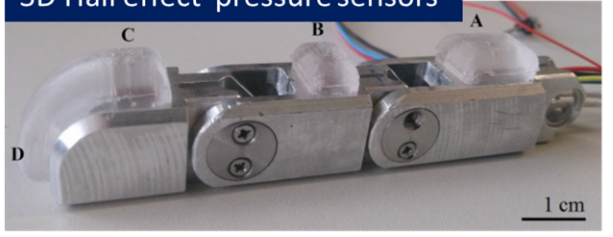
IEEE Trans Magn. vol. 51 (11) 4401104 (2015)
 J.Gaspar et.al, IEEE Trans Magn. Vol.53 (4), 5300204 (2017)

Applications in robotics

The Vizzy hand



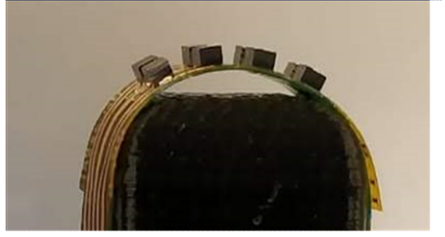
3D Hall effect pressure sensors



Flexible 2D GMR pressure sensors

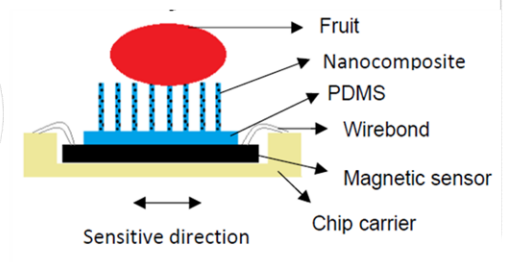
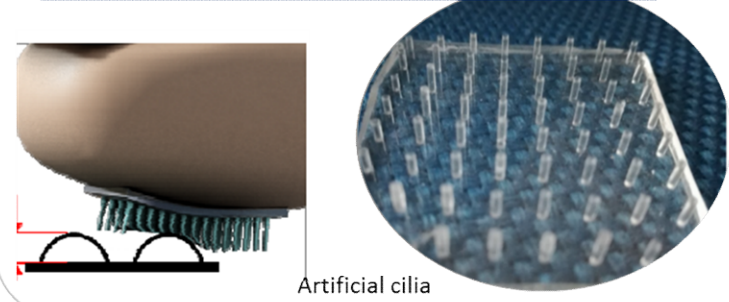


Distributed GMR/TMR sensors



2D MR sensors mounted by flip-chip

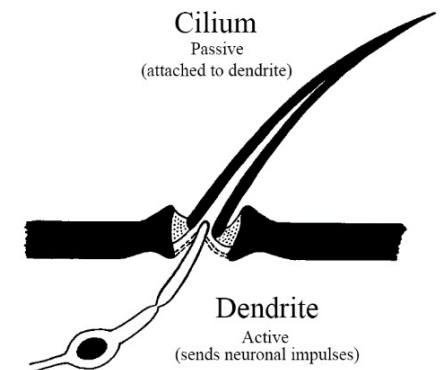
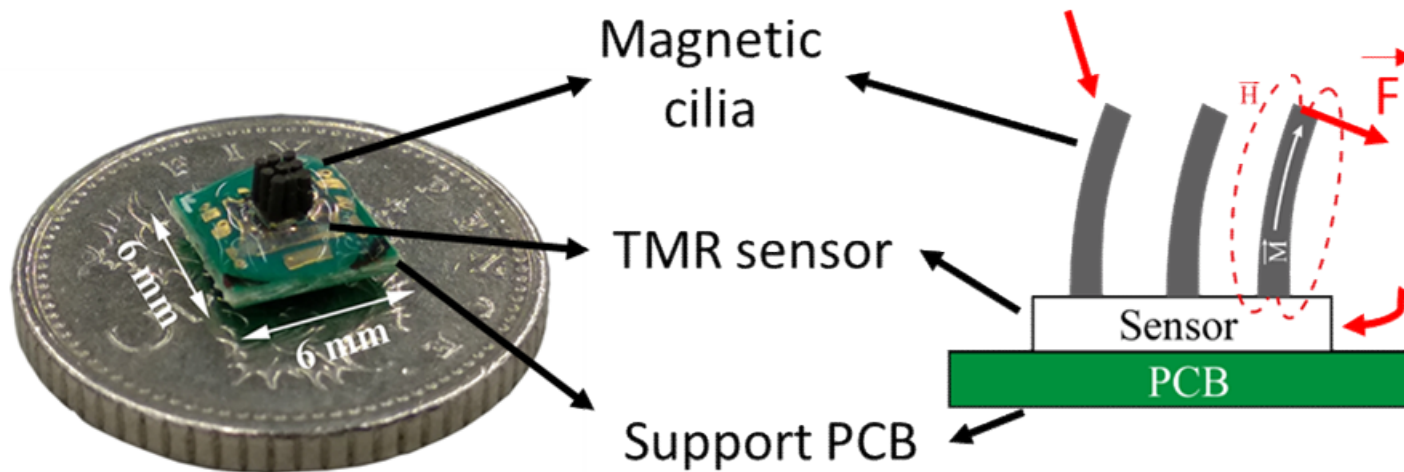
Cilia + 2D GMR tactile and pressure sensors



If no time: move to

Magnetic cilia bending **induces** magnetic profile variation

MR sensor transduces variation into an electrical signal



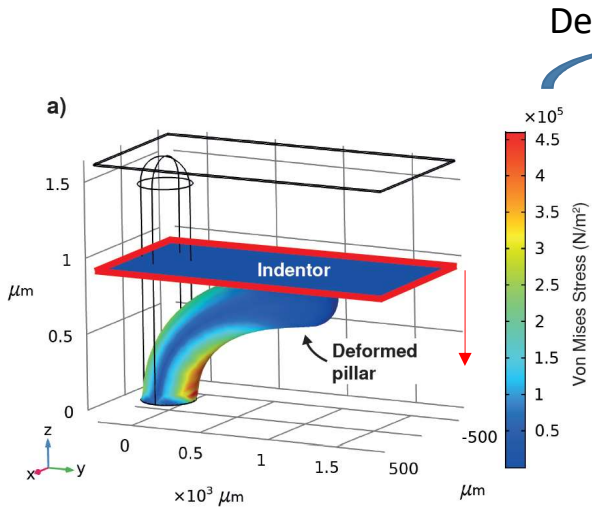
A. Alfadhel and J. Kosel, *Advanced Materials*, 27, 7888–7892, 2015.

P. Ribeiro, et.al. *IEEE Robotics and Automation Letters*, 2, 971–976, 2017.

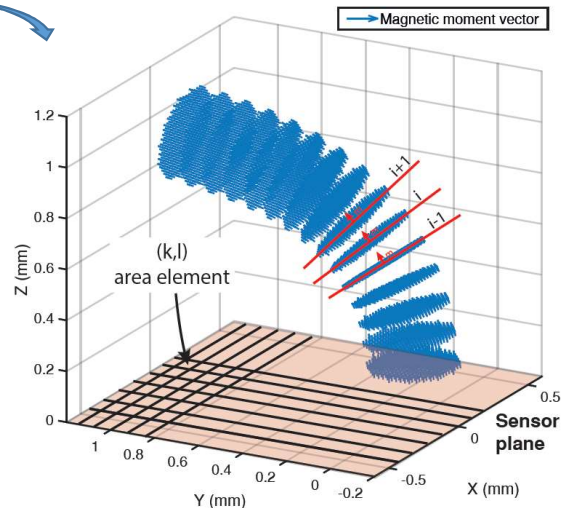
**Mechanical simulation
(FEM – with COMSOL)**

**Magnetic moment
simulation**

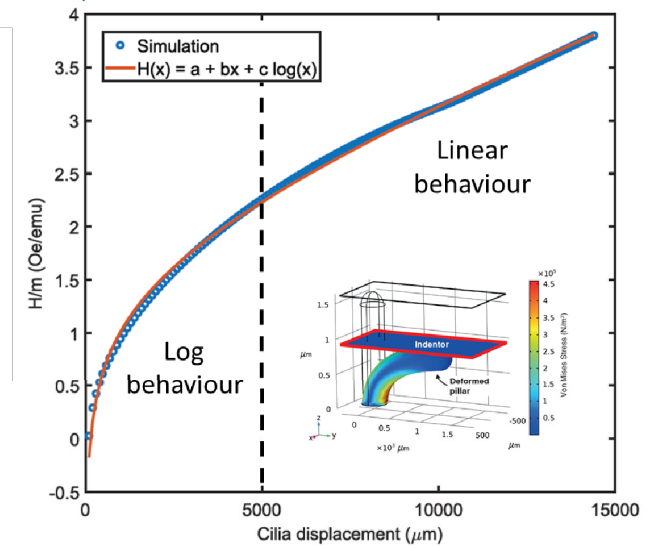
**Magnetic moment
simulation**



Deformation



Magnetic field



Simulation: indenter iteratively lowered against cilia
Steps of 100 μm
Discretized into cross-sections

$$\mathbf{v}_{i-1} = \overrightarrow{i-1, i}; \quad \mathbf{v}_{i+1} = \overrightarrow{i, i+1}$$

$$\mathbf{v}_i = \frac{\mathbf{v}_{i+1} + \mathbf{v}_{i-1}}{2}$$

Estimation of **m** direction

$$\mathbf{H}_j(r_{j,(k,l)}) = \frac{1}{4\pi} \left(\frac{3\mathbf{r}_{j,(k,l)}(\mathbf{m}_j \cdot \mathbf{r}_{j,(k,l)})}{|\mathbf{r}_{j,(k,l)}|^5} - \frac{\mathbf{m}_j}{|\mathbf{r}_{j,(k,l)}|^3} \right)$$

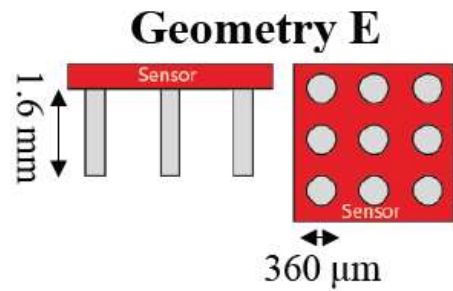
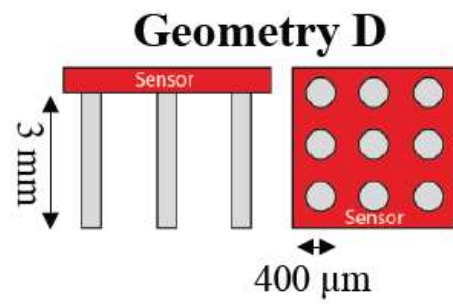
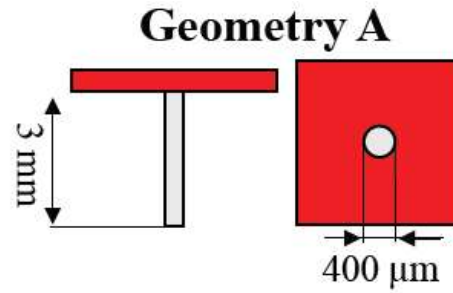
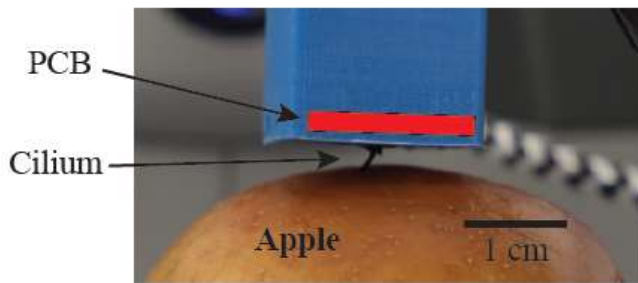
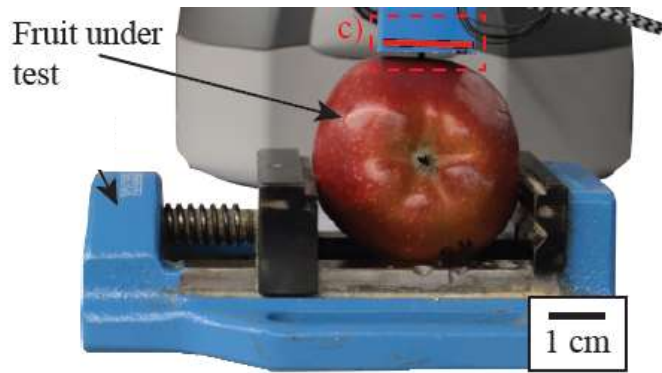
H (x direction) over surface

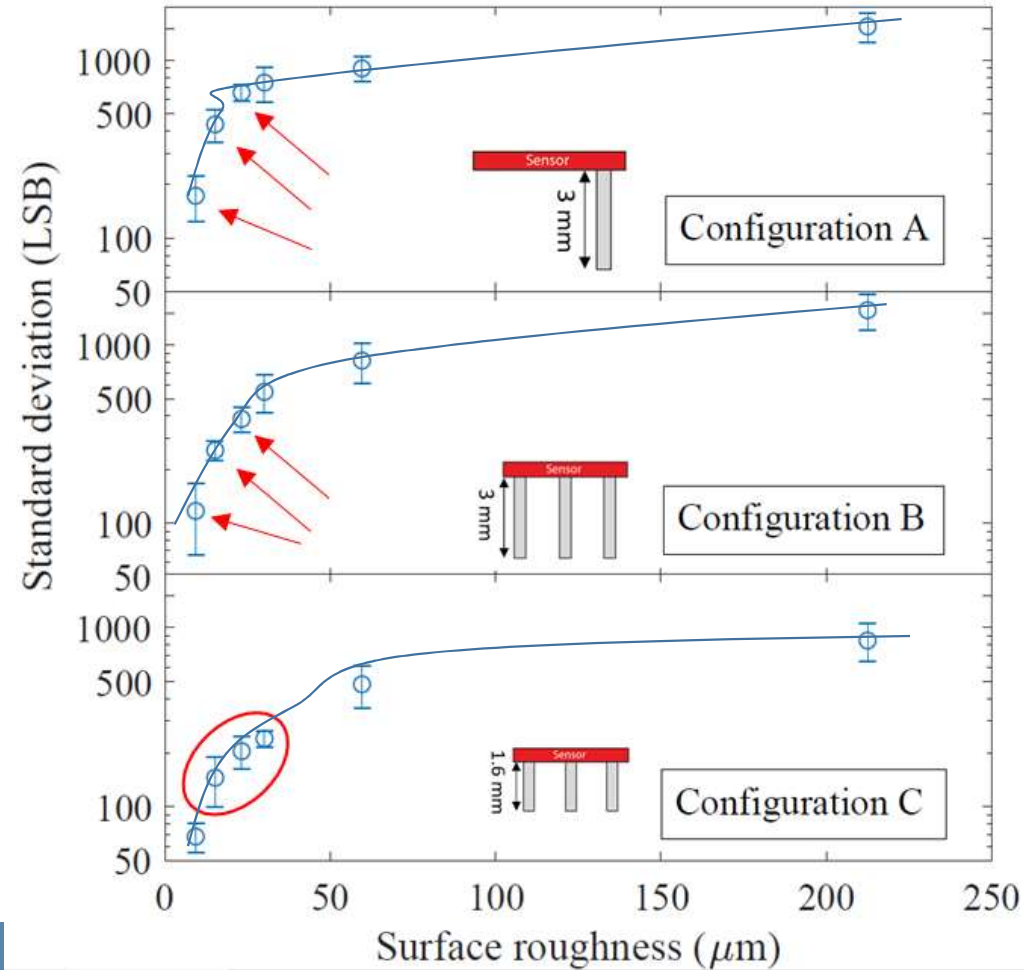
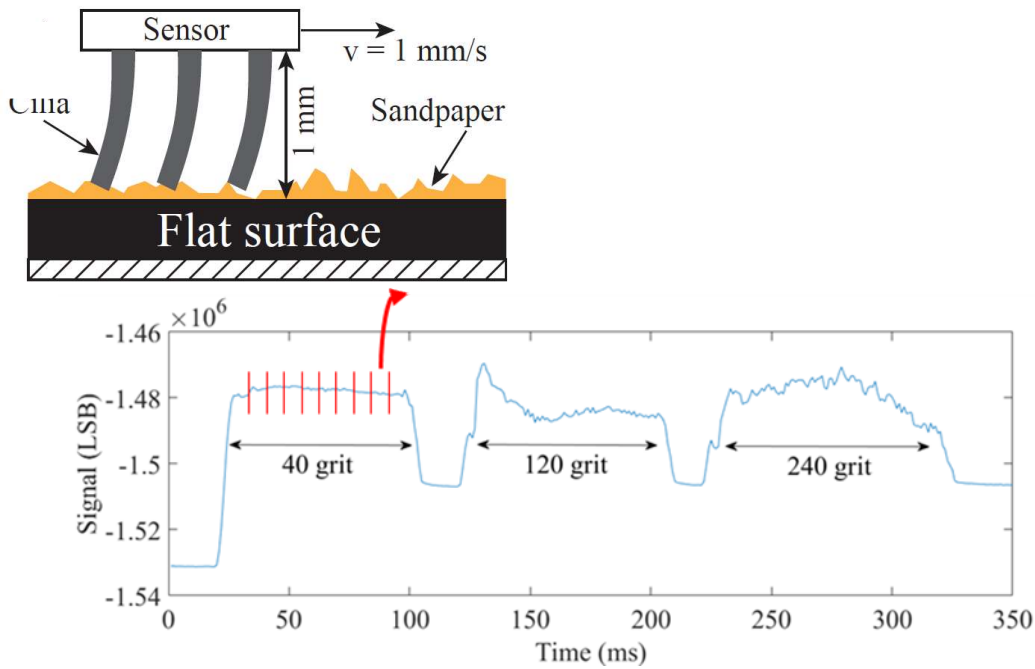
$$\langle \mathbf{H}_{inc} \rangle = \frac{\sum_{k=1}^{N_k} \sum_{l=1}^{N_l} \sum_{j=1}^N \mathbf{H}_j(r_{j,(k,l)})}{N_k N_l}$$

Average field over sensor area

$$\langle H \rangle(x) = ax + b \log(x) + c$$

Best fitting function describing field





- Surface roughness from the signal standard deviation
- **Configuration A and B provide better resolution**
- 5.9 μm resolution



Proof of concept Fruit quality classifier

Braeburn apples

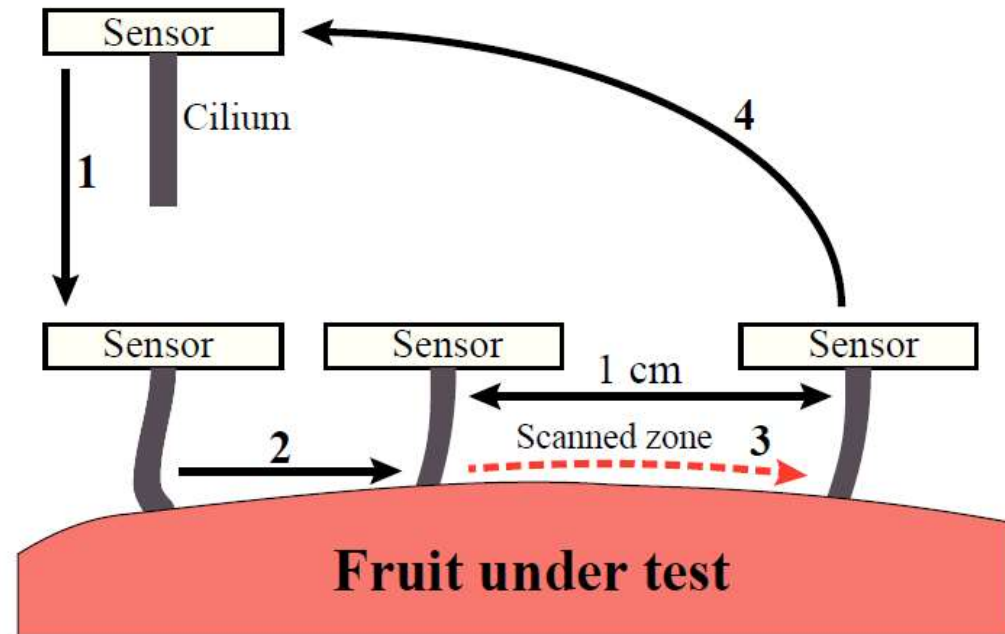
- 12 ripe fruits
- 12 senescent fruits

Sabrina strawberries

- 12 ripe fruits
- 12 senescent fruits

Data acquisition

- Data rate: 1 kSPS
- Scan speed: 1 mm/s
- 10 consecutive scans in each area
- 2 areas per fruit



FRUIT QUALITY SENSING - RESULTS



3 features were extracted from the signal

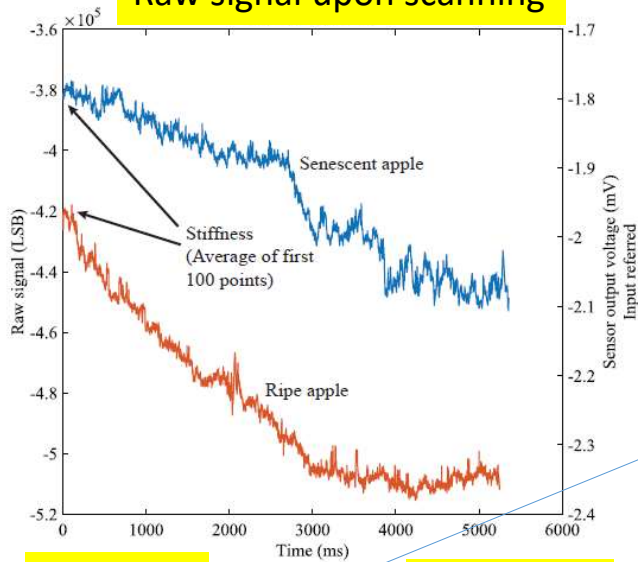
FEATURE	WHAT IS MEASURED	PHYSICAL CHARACTERISTIC
Stiffness (E)	Sensor signal with achieved contact	Fruit hardness
Waviness (S)	Std. deviation of 100 point moving average	Deformation over fruit surface
Roughness (R)	Std. deviation of high-pass filtered (f > 150 Hz) signal	Fruit surface texture

Fruit can be classified into two classes

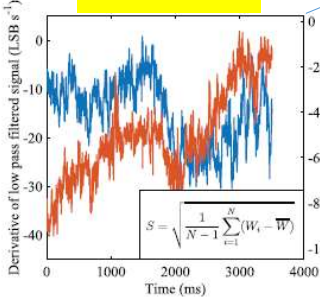
Ripe

Senescent

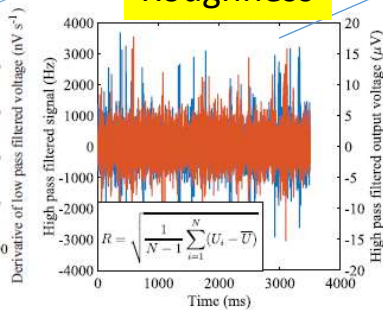
Raw signal upon scanning



Waviness



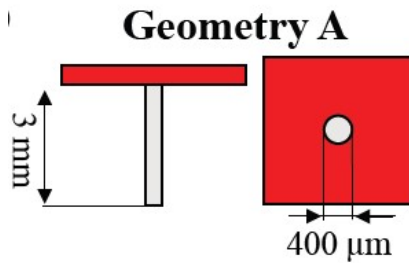
Roughness



$$S = \sqrt{\frac{1}{N-1} \sum_{i=1}^N (W_i - \bar{W})^2}$$

$$R = \sqrt{\frac{1}{N-1} \sum_{i=1}^N (U_i - \bar{U})^2}$$

FRUIT QUALITY SENSING - RESULTS



Stiffness (E) \longrightarrow Fruit hardness

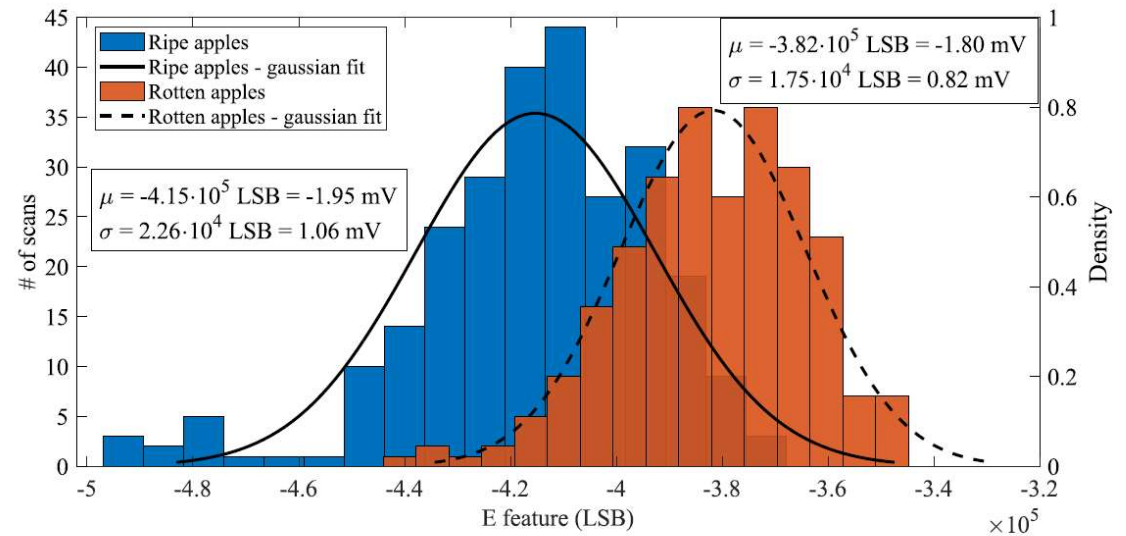
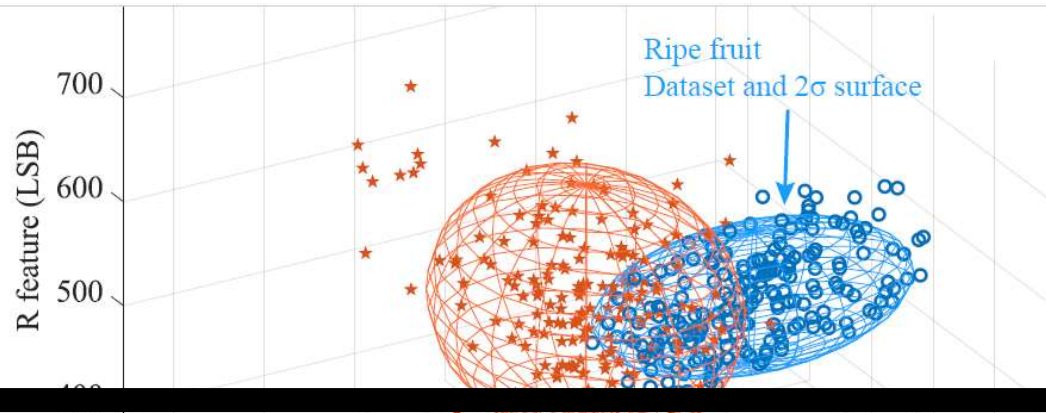


Figure 6.4: Computed E parameter histogram from all scans of apples scanned using a geometry A ciliary sensor.

Gaussian classifier (Gaussian Naïve Bayes)



Combining R, S, E

Sensor	Fruit	1 feature (E)	2 features ($E + R$)	3 features ($S + E + R$)
B	Apple	0.83	0.92	0.96
	Strawberry	0.63	0.79	0.71
D	Apple	0.71	0.88	0.88
	Strawberry	0.67	0.67	0.71
E	Apple	0.58	0.71	0.71
	Strawberry	0.63	0.83	0.83

Table 6.3: Accuracy vs number of features used for classification with Gaussian Naïve Bayes algorithm.

FRUIT QUALITY SENSING - RESULTS



Apple



Strawberry

Conf. A



$h = 3 \text{ mm}$
 $\phi = 400 \mu\text{m}$

	True positive	True negative	Accuracy
Naïve Bayes	11/12	12/12	0.96
Random Forest	10/12	12/12	0.92

	True positive	True negative	Accuracy
Naïve Bayes	7/12	10/12	0.71
Random Forest	8/12	11/12	0.79

Conf. B



$h = 1.6 \text{ mm}$
 $\phi = 320 \mu\text{m}$

	True positive	True negative	Accuracy
Naïve Bayes	10/12	11/12	0.88
Random Forest	10/12	11/12	0.88

	True positive	True negative	Accuracy
Naïve Bayes	10/12	7/12	0.71
Random Forest	10/12	10/12	0.83

Conf. C



$h = 3 \text{ mm}$
 $\phi = 400 \mu\text{m}$

	True positive	True negative	Accuracy
Naïve Bayes	9/12	8/12	0.71
Random Forest	9/12	11/12	0.83

	True positive	True negative	Accuracy
Naïve Bayes	10/12	10/12	0.83
Random Forest	10/12	10/12	0.83

“From farm to fork”

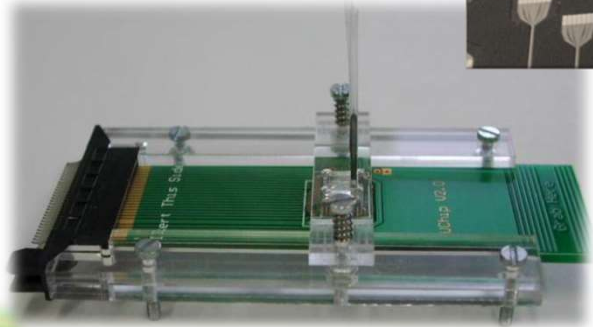
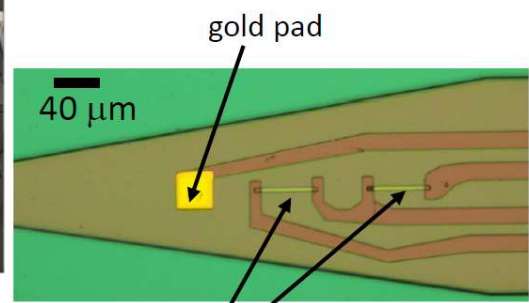
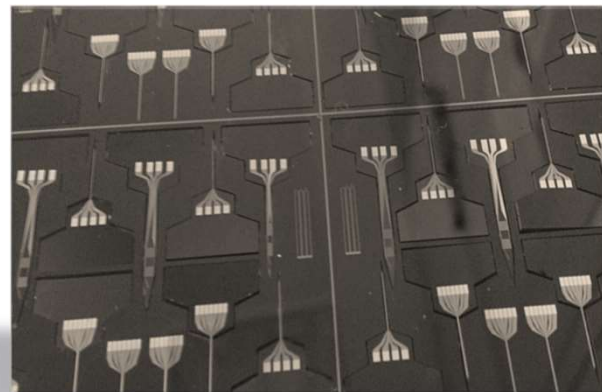
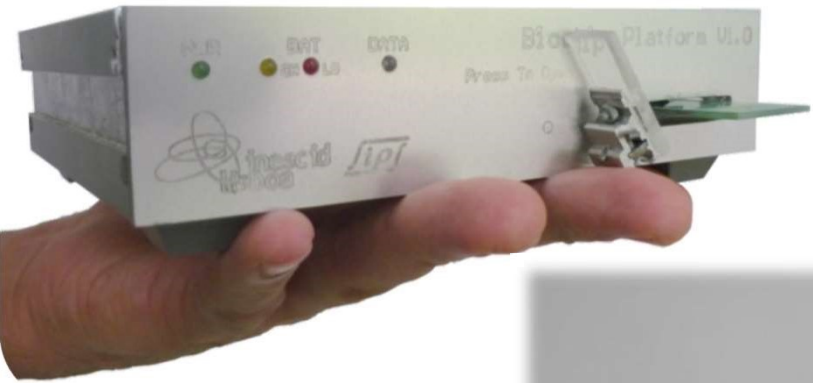


Final food inspection

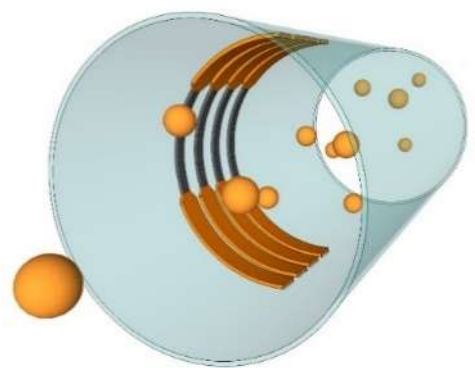
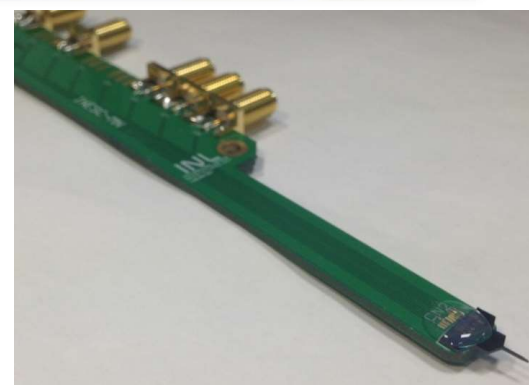
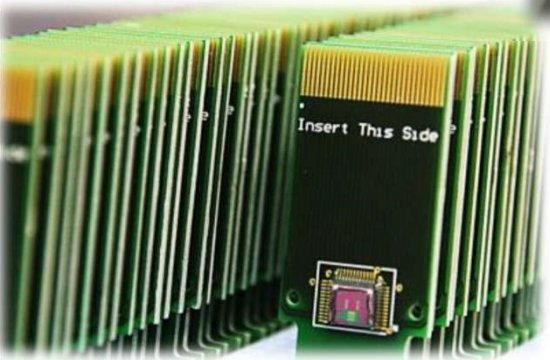


If no time:
move to

Magnetic Biosensors and biomedical interfaces



Needle sensors
Flexible MR Sensors

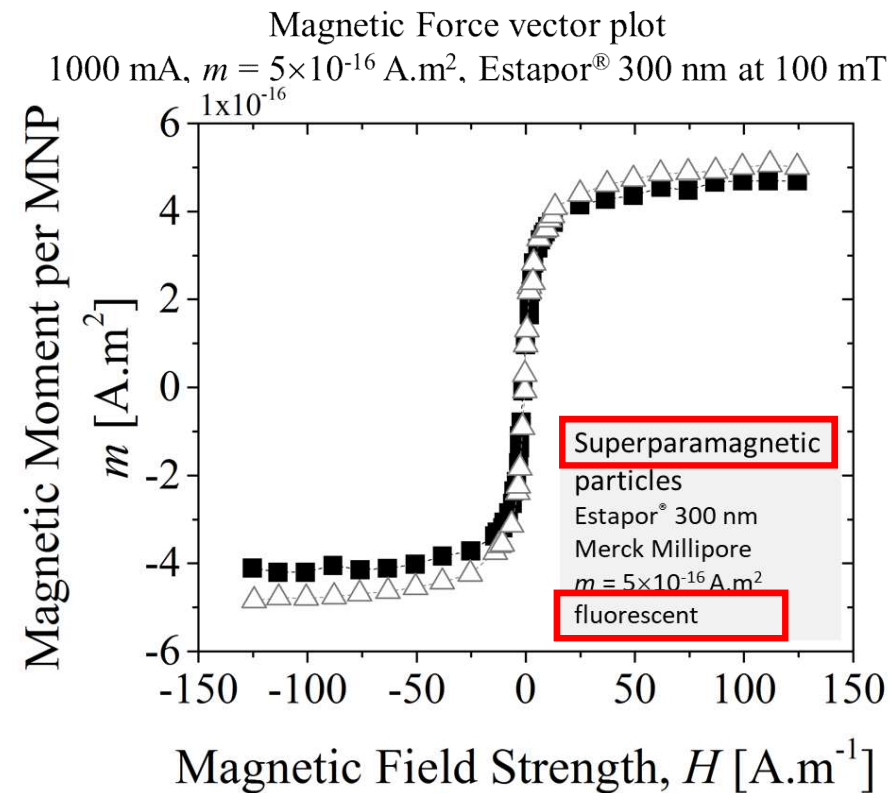
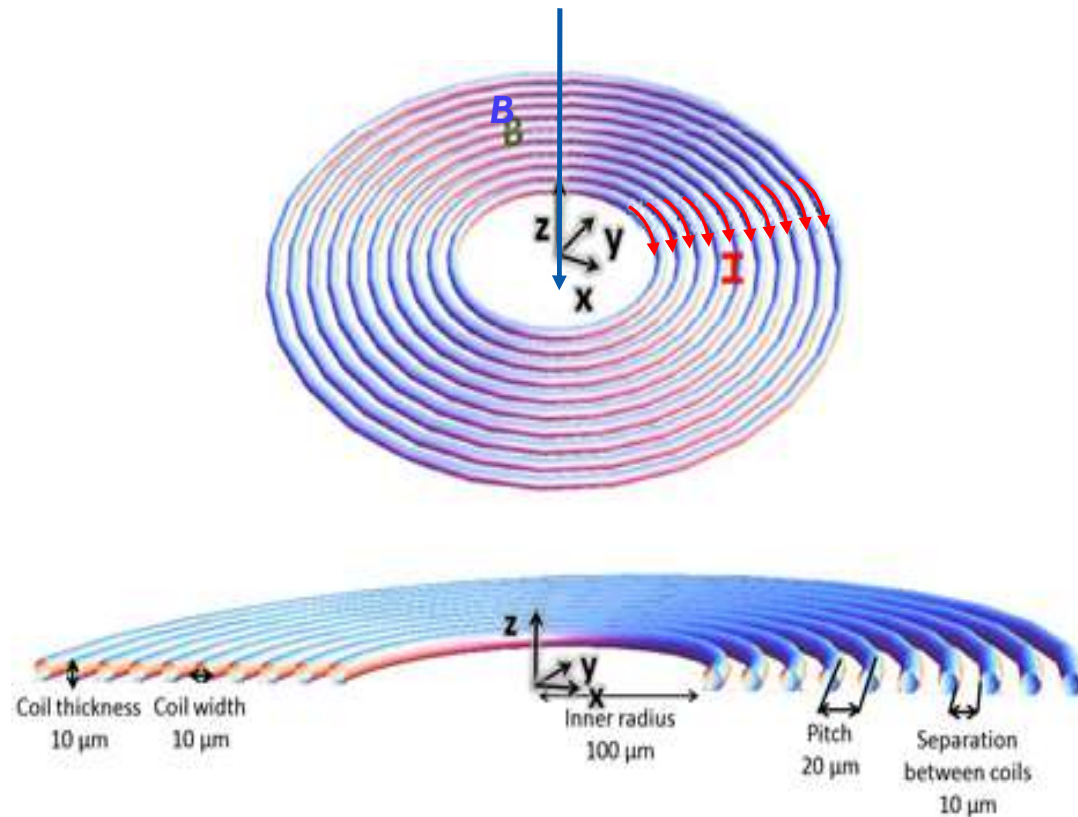


If no time:
move to

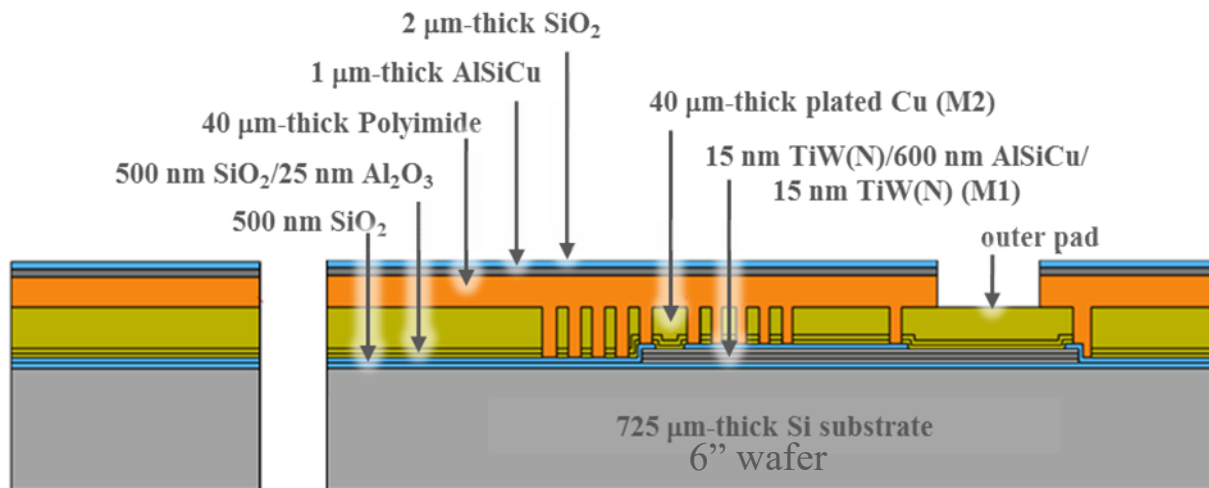
Magnetic trap

Magnetic force exerted on MNP: $F_{mag} = \nabla (m \cdot B)$

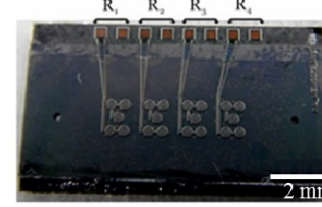
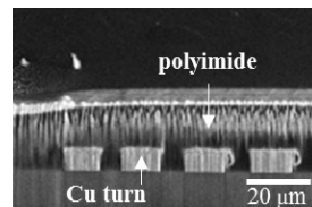
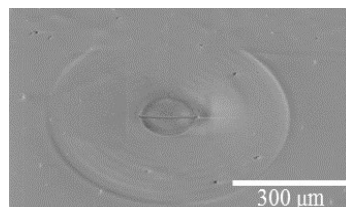
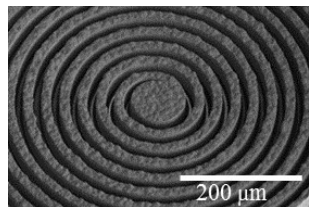
magnetic moment m , magnetic field B



Microfabrication



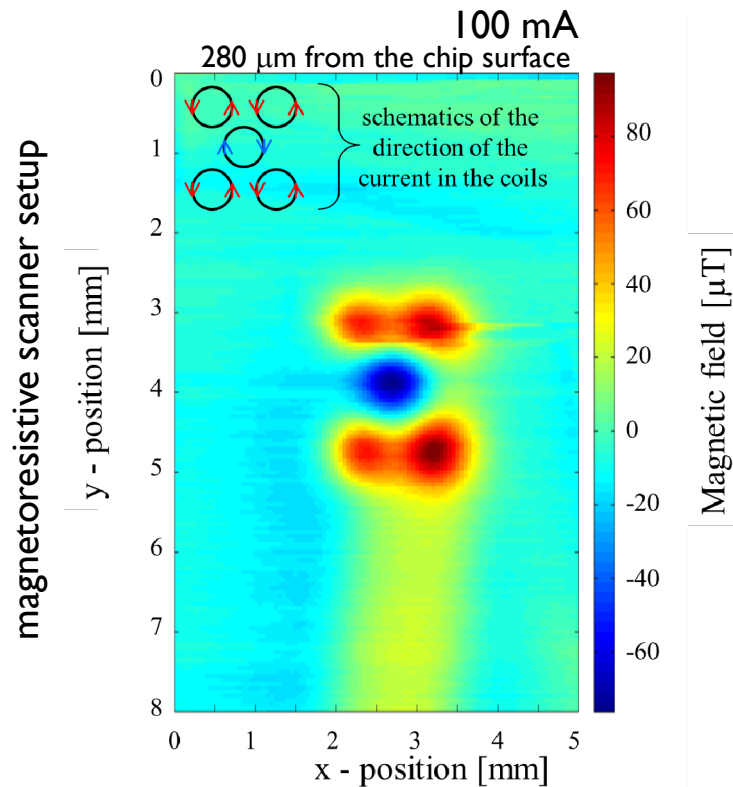
1. PECVD 500 nm SiO_2 : 6'' wafer
2. magnetron sputtering 15 nm TiW(N)/600 nm AlSiCu/15 nm TiW(N) : bottom electrode (M1 layer)
3. optical lithography
4. etching
 - This M1 film also connects the center of the coils to the contact pad
5. RF sputtering SiO_2 500 nm / Al_2O_3 25 nm
 - passivation layer to insulate the coil from the bottom electrode
6. optical lithography
7. electroplating 40 μm of Cu (M2 layer)
8. spin coating 40 μm polyimide
 - passivation
9. sputtering 1 μm AlSiCu
 - ensures an optimum optical contrast for the detection of the fluorescence in the MNP
10. sputtering 2 μm SiO_2
 - guarantees the planar surface required for the magnetic trapping and in the future, to promote probe linking
11. RIE to open 250 μm wide vias for contact pads



Silvério et.al., Micromachines 10(9):607 (2019);

Silverio et. Al., IEEE Trans Magn. 53 (11) 5100806 (2017)

Magnetic Field Mapping



Magnetic Tunnel Junction (MTJ), sensitivity
 $0.04 \text{ V}\cdot\text{mT}^{-1}$, dimension $91 \times 14.5 \mu\text{m}^2$

The vertical magnetic field over the **central coil** is **opposite** to the vertical field in the **4 outer coils**

- favorable for particle trapping and cell concentration

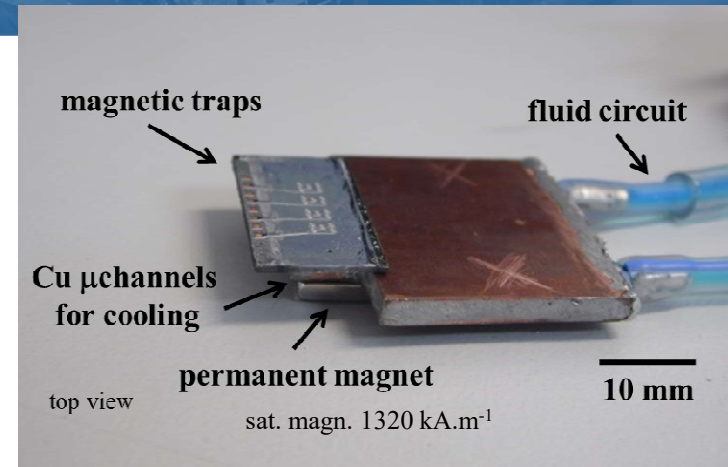
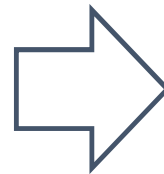
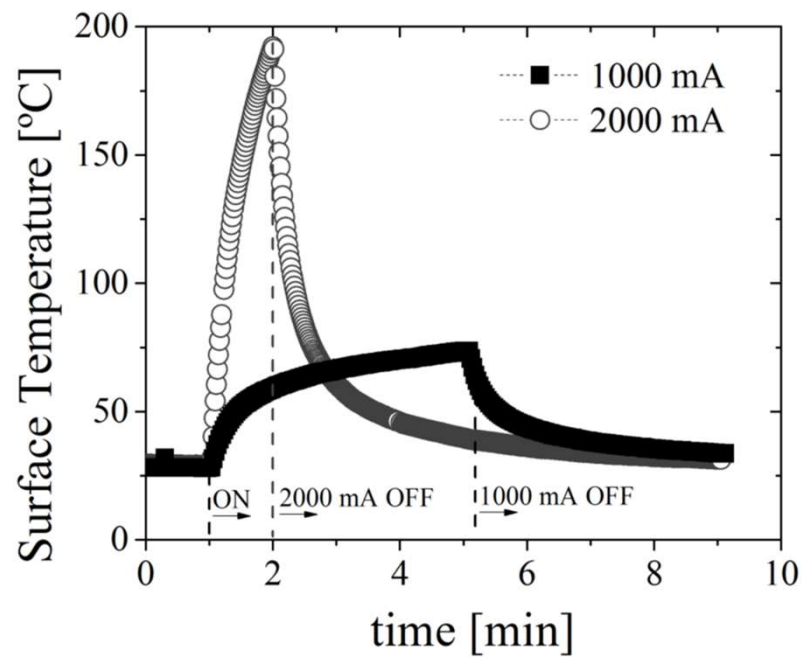
The field generated by 100 mA was measured to range between -70 to $+90 \mu\text{T}$

1000 mA actuation + PM field

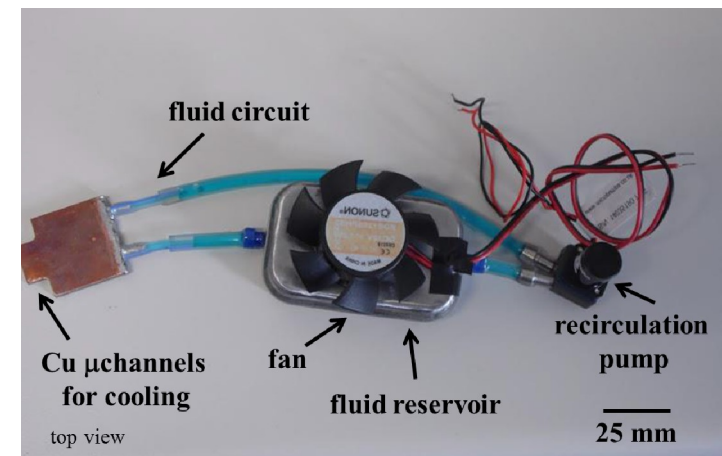
- larger magnetic fields: -1500 to $+3000 \mu\text{T}$
- sufficient to generate a magnetic force to deflect the MNP trajectories and trap them

Thermal response

- Joule heating \rightarrow flow cooling



200 μ m deep triangular microchannels enclosed on the copper block



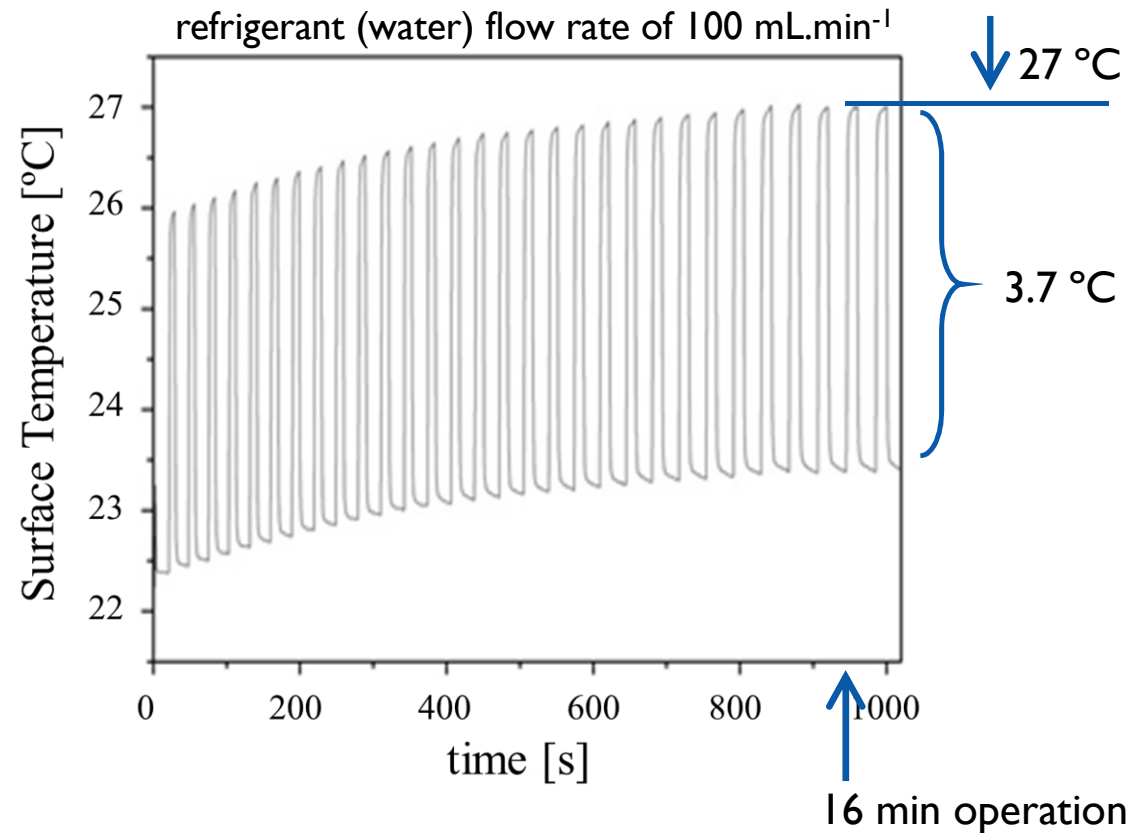
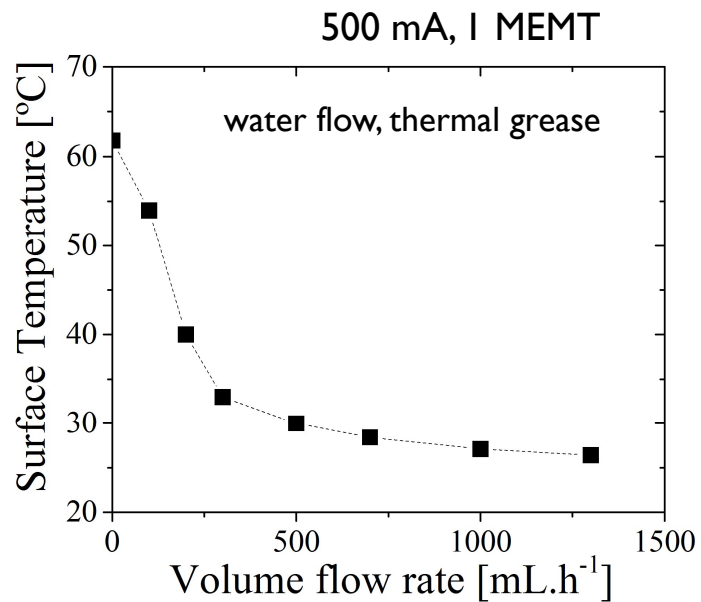
Silvério et.al., Micromachines 10(9):607 (2019);

Silverio et. Al., IEEE Trans Magn. 53 (11) 5100806 (2017)

Thermal response

pulsed current: 500 mA

8 s ON / 15 s OFF



Silvério et.al., Micromachines 10(9):607 (2019);

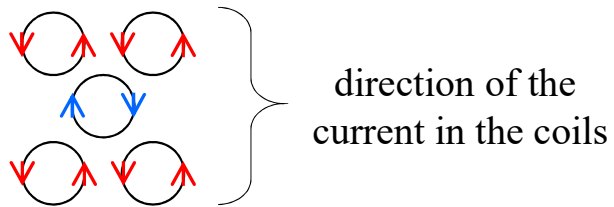
Silverio et. Al., IEEE Trans Magn. 53 (11) 5100806 (2017)

Tombelli, et.al., Analytical and Bioanalytical Chemistry 414 (10), 3243 (2022)

MNP Trapping and concentration

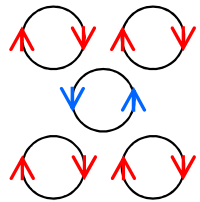
16 pulses @ +750 mA

1 s ON + 2 s OFF + 1 s ON + ...

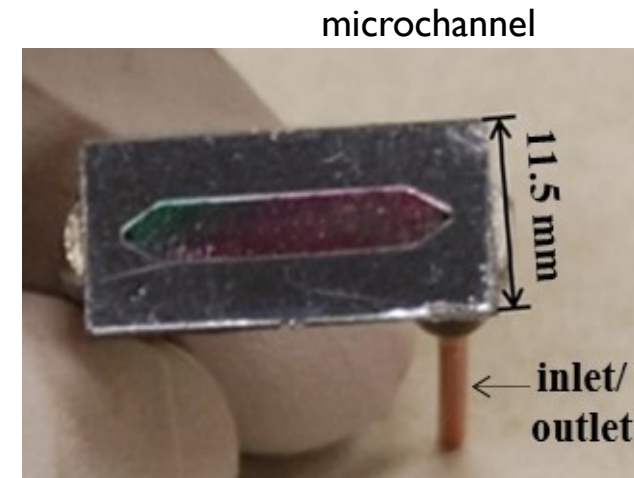
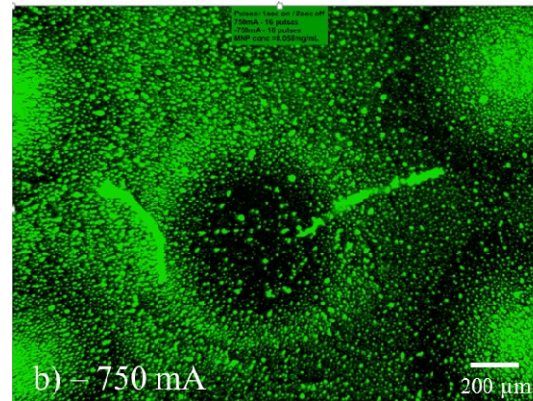
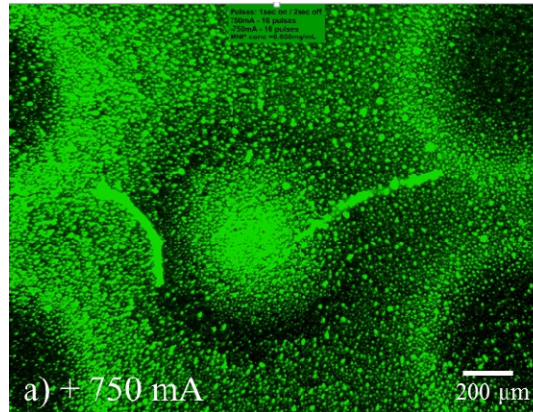


16 pulses @ -750 mA

1 s ON + 2 s OFF + 1 s ON + ...



$$T_{surf,max} = 3 \text{ } ^\circ\text{C}$$



MNP concentration
0.058 mg.mL⁻¹

Silvério et.al., Micromachines 10(9):607 (2019);

Silverio et. Al., IEEE Trans Magn. 53 (11) 5100806 (2017)

Tombelli, et.al., Analytical and Bioanalytical Chemistry 414 (10), 3243 (2022)

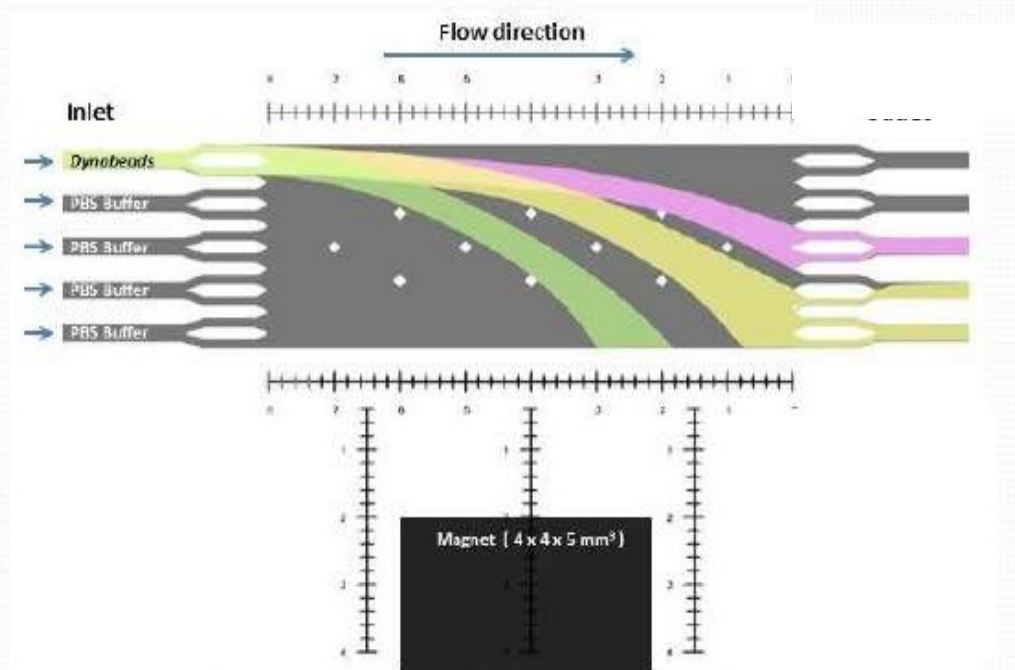
Magnetic separation

volume magnetite \downarrow magnetic susceptibility (particle minus environment) \downarrow

$$\mathbf{F}_{mag} \propto \frac{V_m \cdot \Delta\chi}{\mu_0} (\mathbf{B} \cdot \nabla) \mathbf{B}$$

\nwarrow magnetic field strength
 \nearrow magnetic field gradient

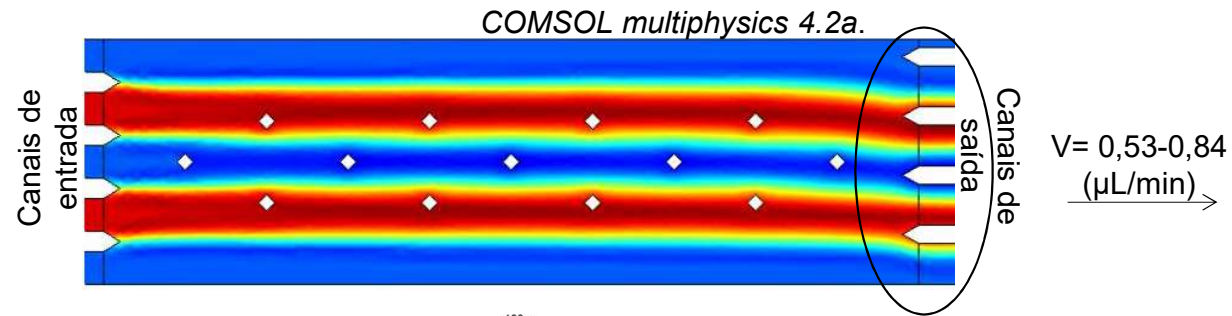
- Flow rate**
- 4.63 mm/s
 - 2.31 mm/s
 - 0.93 mm/s



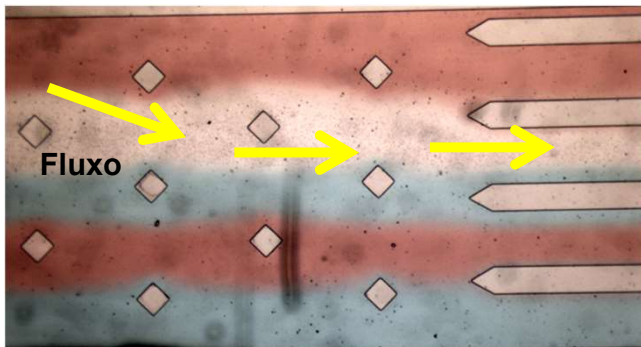
Tarn, Pamme, JMMM 2009, 4115.

Magnetic separation

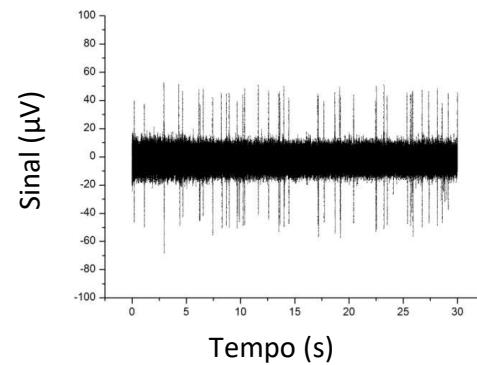
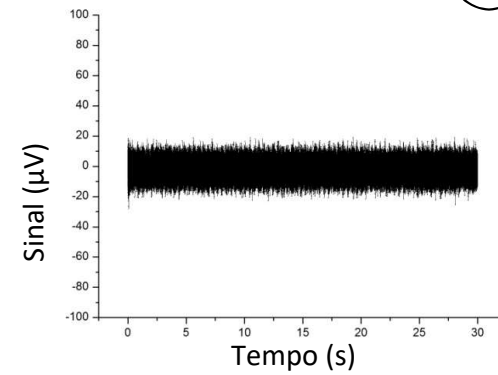
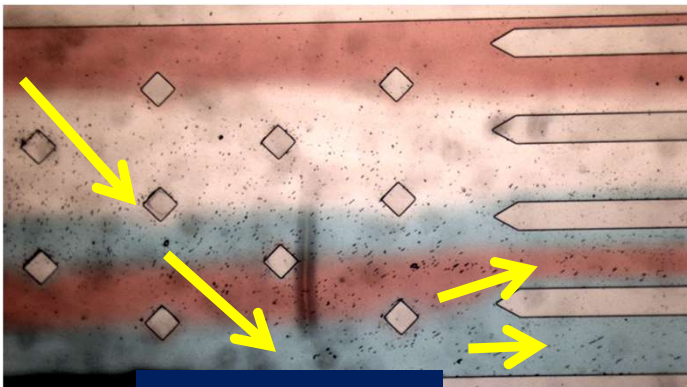
$V = 0,5 \mu\text{L}/\text{min}$



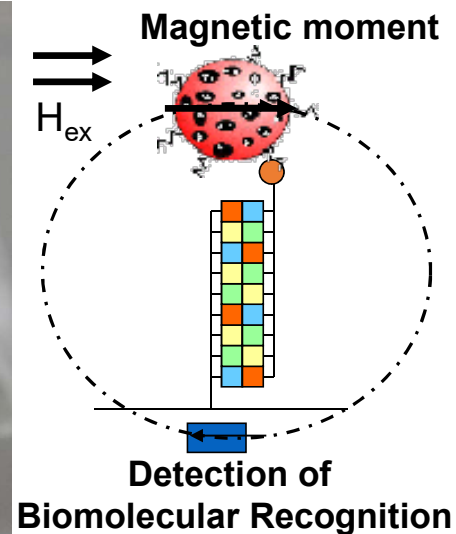
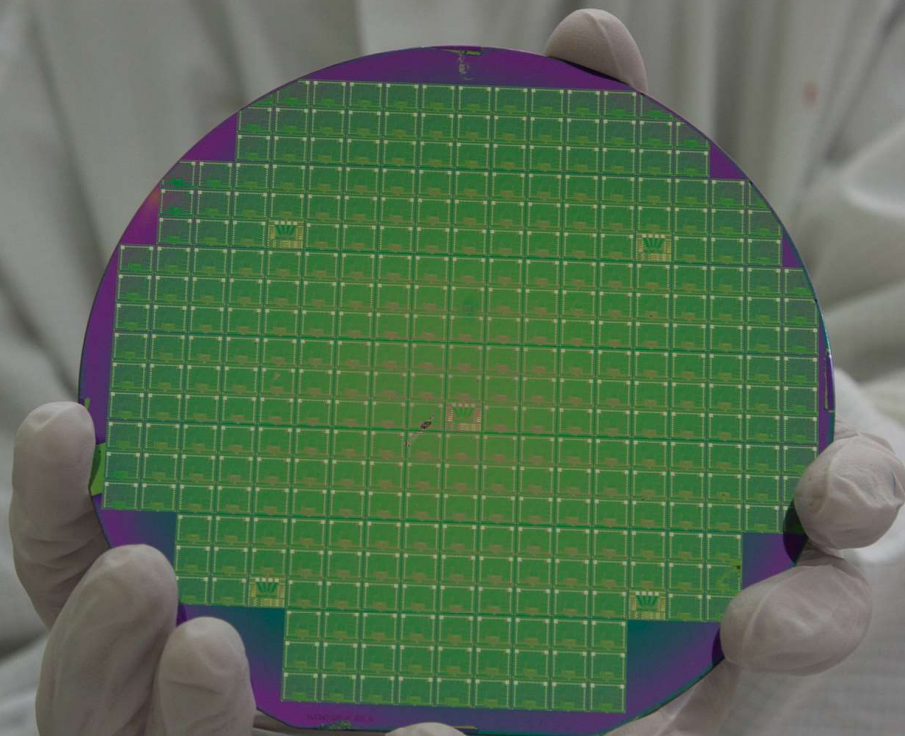
Particle inlet



Particle inlet

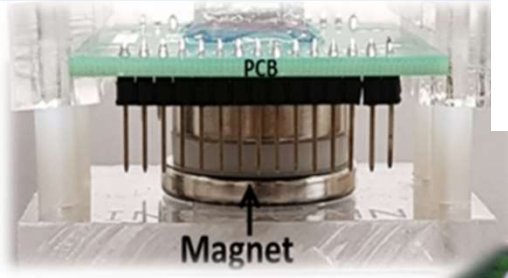


Magnetic biosensors

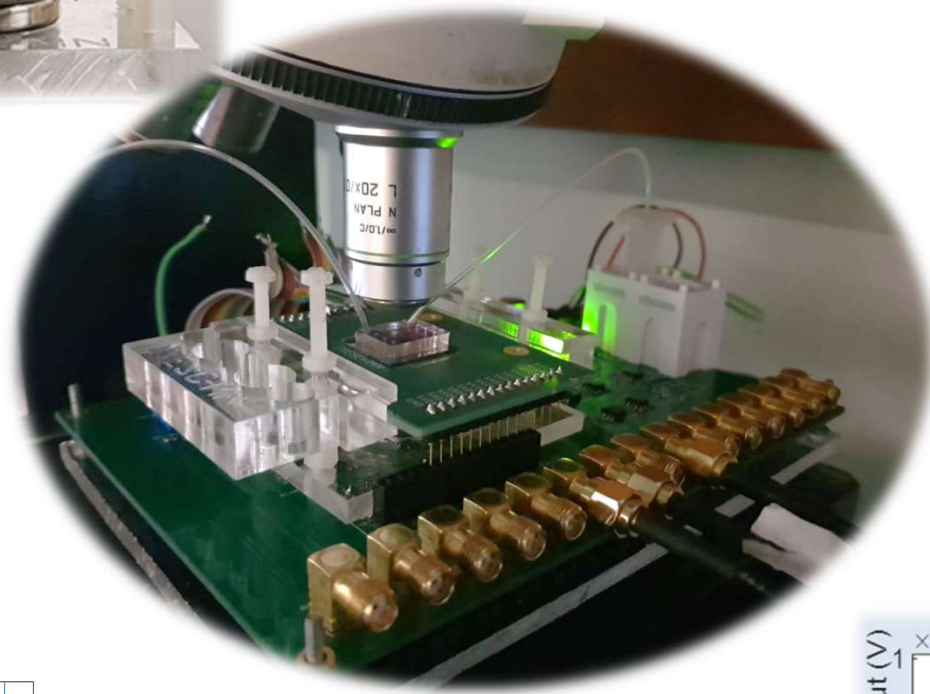


Biosensors and Bioelectronics, 210, 114302 (2022),
Lab-on-Chip 18, 2593-2603 (2018);
Trends in Biotechnology, August 2004
IEEE Magnetics Letters, 10 (1) (2019);
Anal. Bioanal. Chem. (2019) 411, pp. 1839 (2019);
ACS Nano 11 (11), pp 10659–10664 (2017)
Lab-on-Chip, 11 (13), 2255 – 2261 (2011)
Analytical Methods, 8, 119-128 (2016);
Lab-on-Chip, 2012, 12 (3), 546 – 557 (2011)
Biosensors and Bioelectronics 11, 100149, (2022)

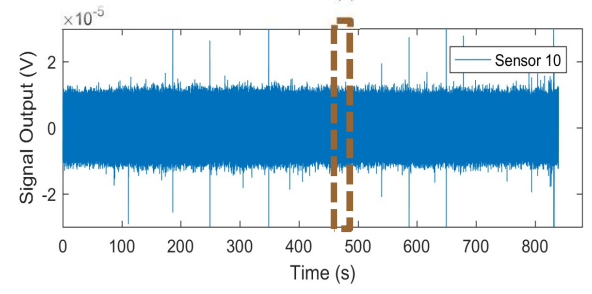
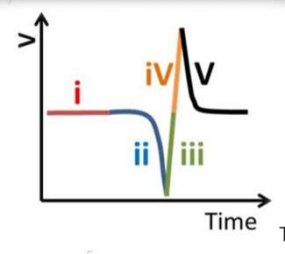
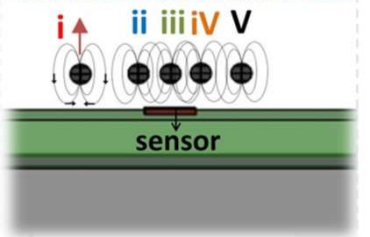
Labels magnetization



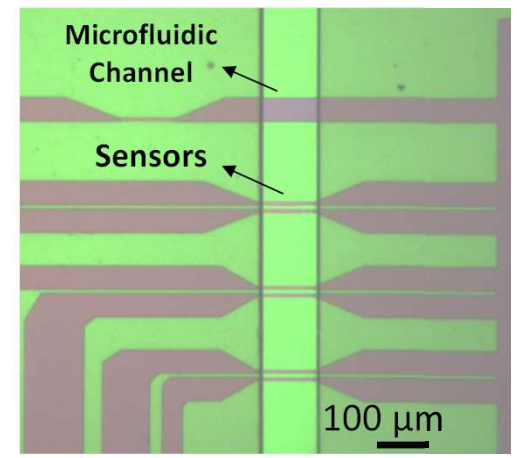
Magnetic cytometer



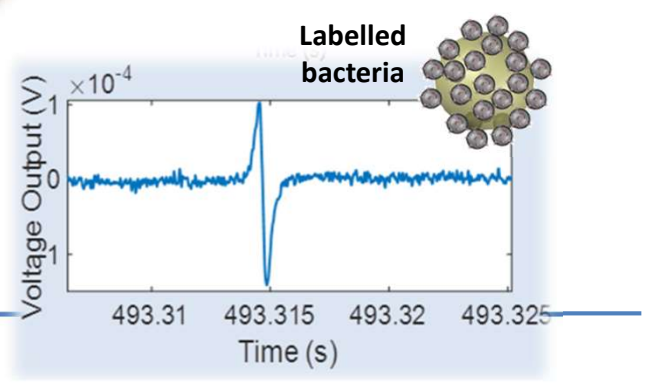
Detection principle



Microfluidics technology



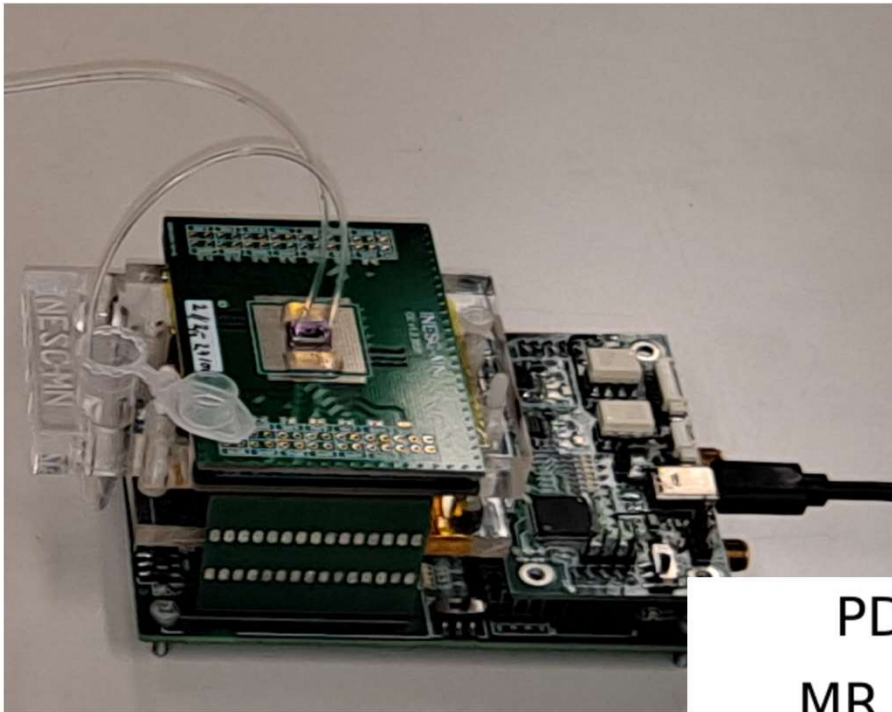
Detection signals



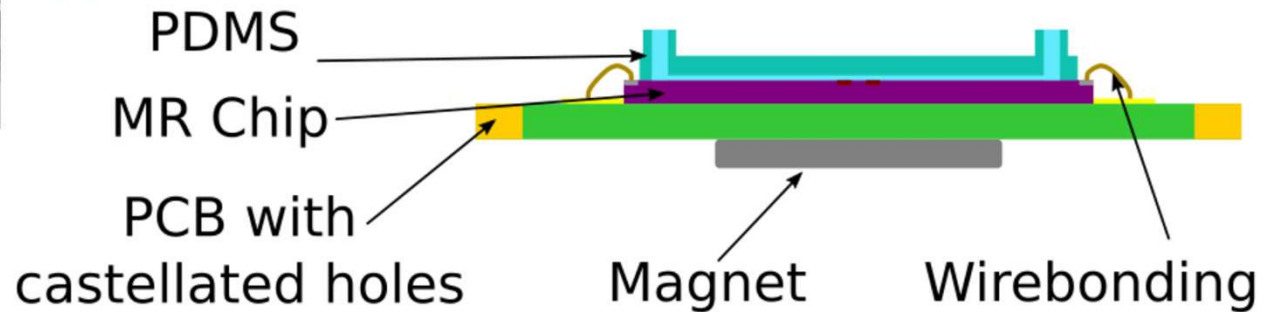
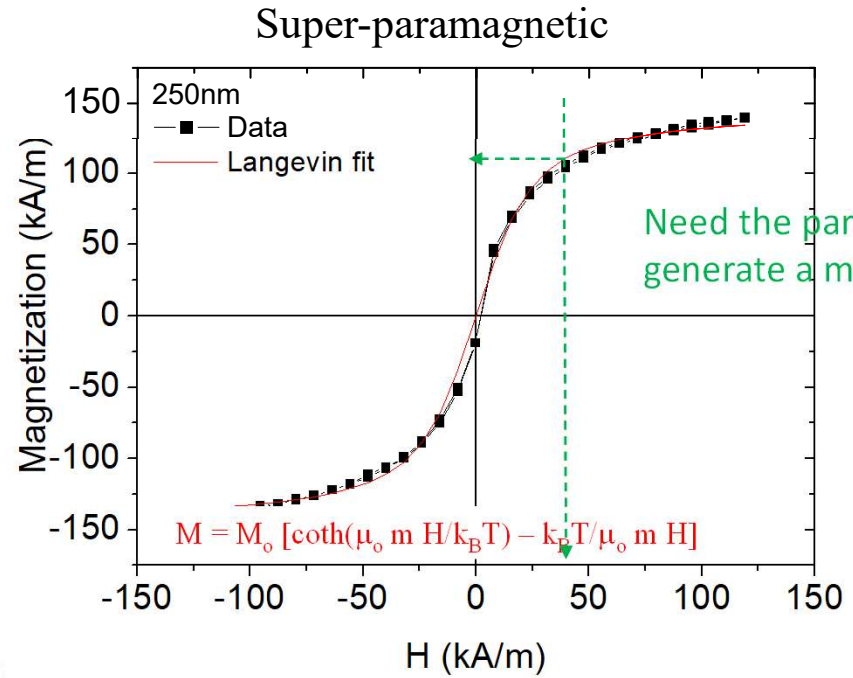
Lab-on-Chip, 11 (13), 2255 – 2261 (2011)

Freitas et.al., Lab-on-Chip, 2012, 12 (3), 546 – 557

Magnetic Labels



Particles typically used in bio-separation

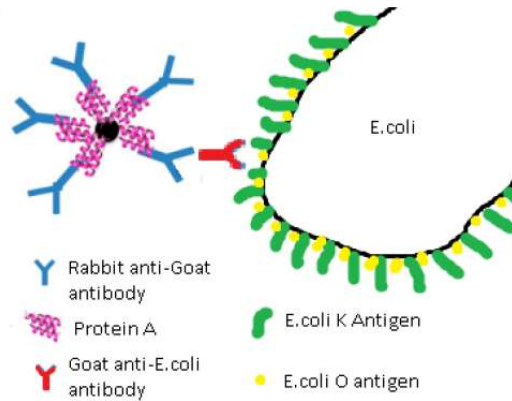


Lab-on-Chip, 11 (13), 2255 – 2261 (2011)

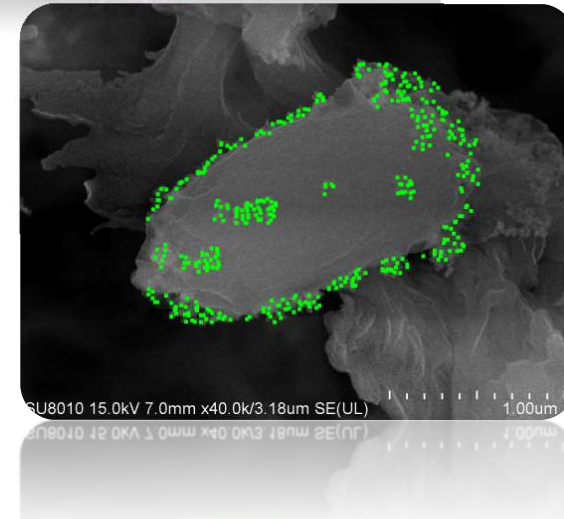
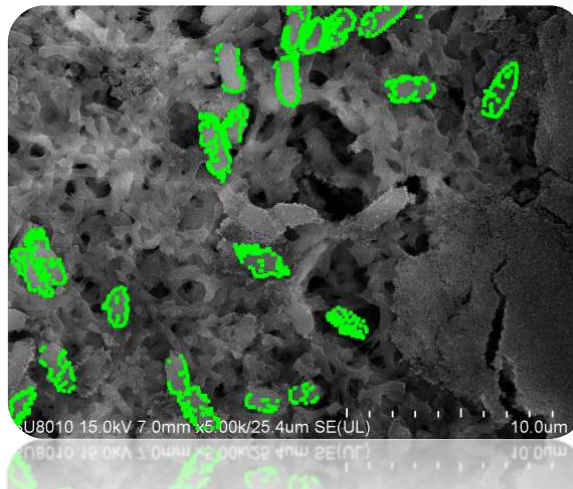
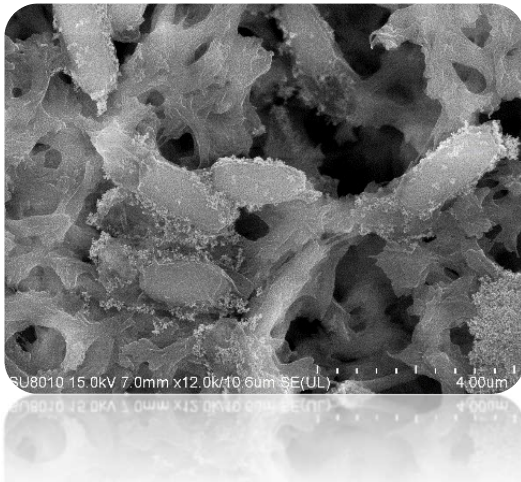
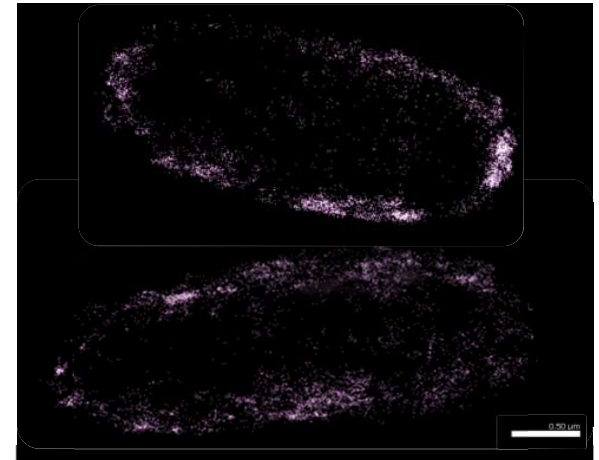
Freitas et.al., Lab-on-Chip, 2012, 12 (3), 546 – 557

Challenges – quantification

- 100nm magnetic particles coated with protein A;
- Rabbit α -goat Ab \rightarrow More affinity to protein A;
- Goat α -*E.coli* Ab \rightarrow Already tested by IF;
- Special SEM processing without organic solvents;



Adapted from Fernandes et al. (2014)



On-site magnetic screening tool for rapid detection of hospital bacterial infections: Clinical study with *Klebsiella pneumoniae* cells

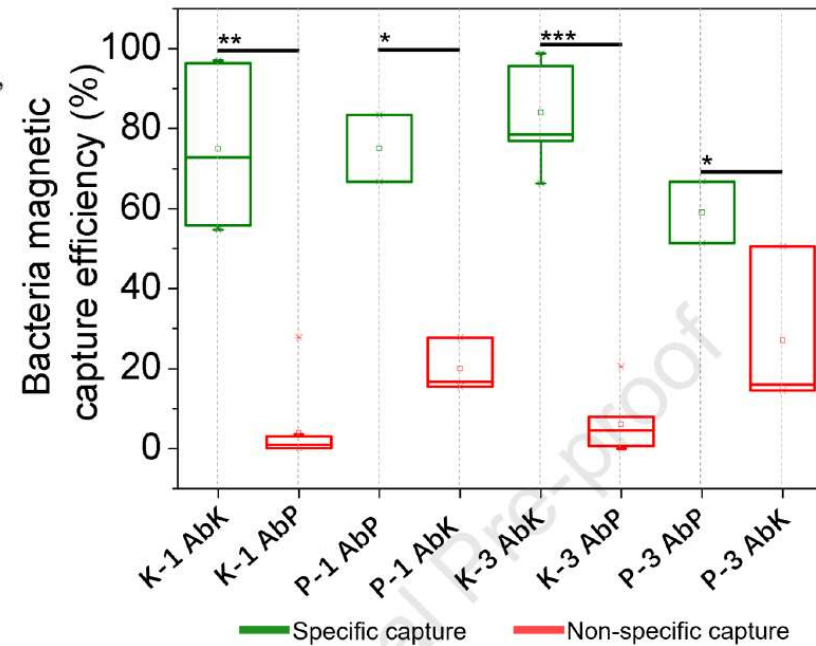
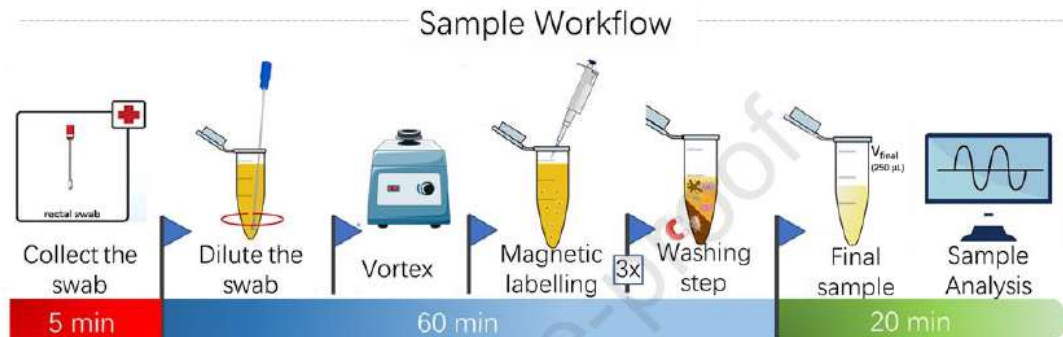
Ana R. Soares^{a,b,*}, R. Afonso^{b,c}, V.C. Martins^a, C. Palos^d, P. Pereira^d, Diogo M. Caetano^{b,c}, Davide Carta^{a,b}, S. Cardoso^{a,b}

^a Instituto de Engenharia de Sistemas E Computadores – Microsistemas e Nanotecnologias (INESC MN), Rua Alves Redol 9, 1000-029, Lisbon, Portugal

^b Instituto Superior Técnico, Universidade de Lisboa, Av. Rovisco Pais 1, 1049-001, Lisbon, Portugal

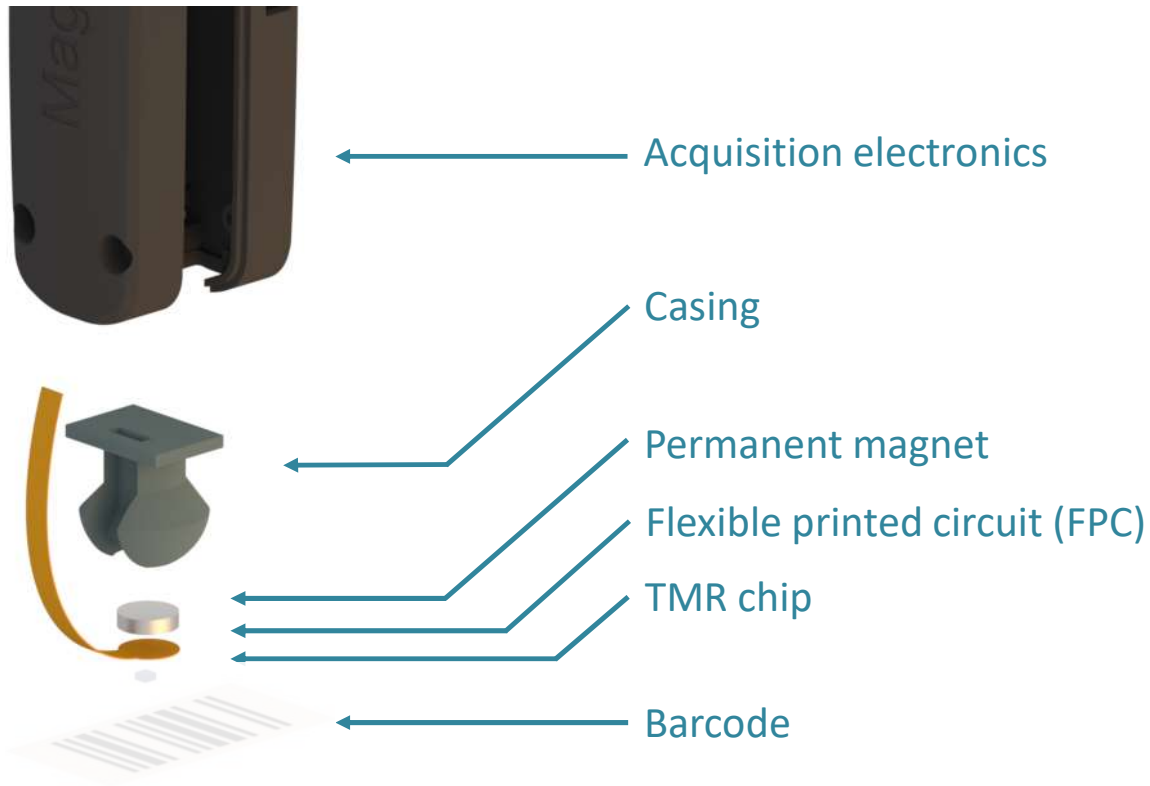
^c Instituto de Engenharia de Sistemas E Computadores - Investigação e Desenvolvimento, Rua Alves Redol 9, 1000-029, Lisbon, Portugal

^d HBA – Hospital Beatriz Ângelo, Av. Carlos Teixeira 3, 2674-514, Loures, Portugal



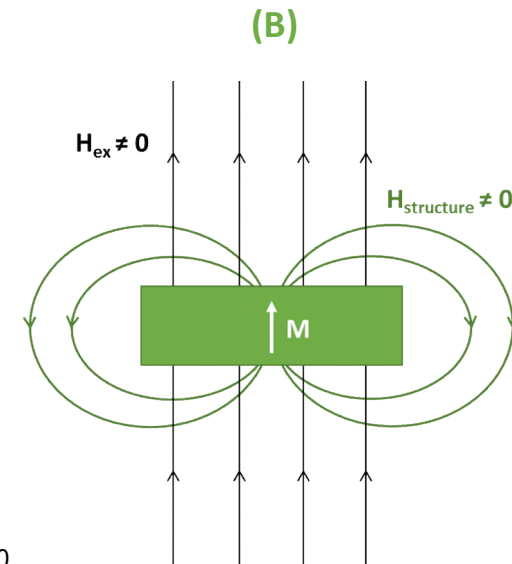
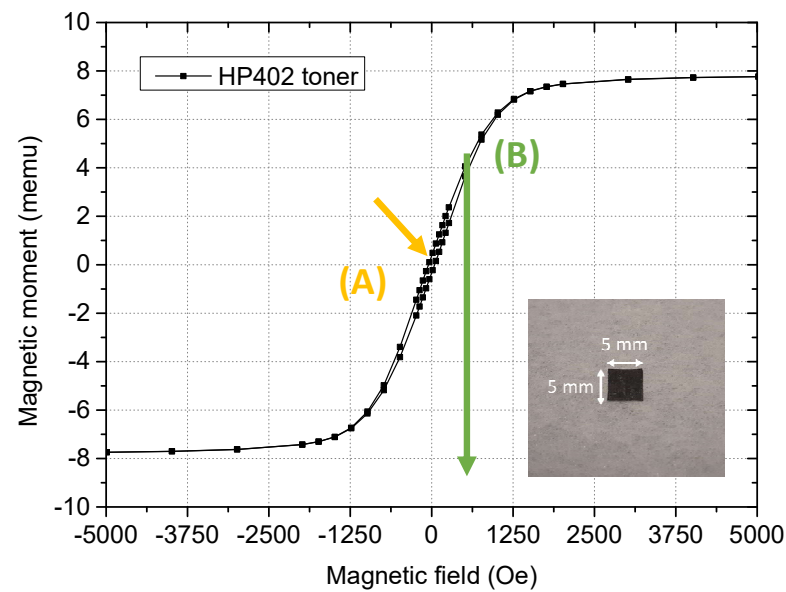
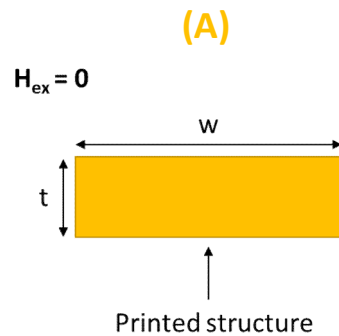
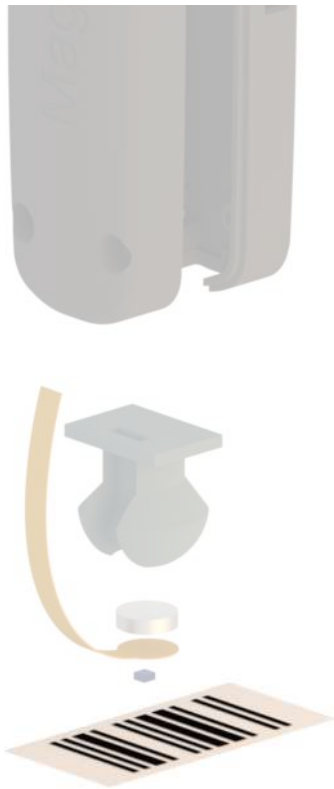
If no time: move to

Applications in scanners



Swipe reader: printed barcode

Regular laserjet toners contain ferromagnetic ($\text{Fe}_3\text{O}_4/\text{Fe}_2\text{O}_3$) nanoparticles



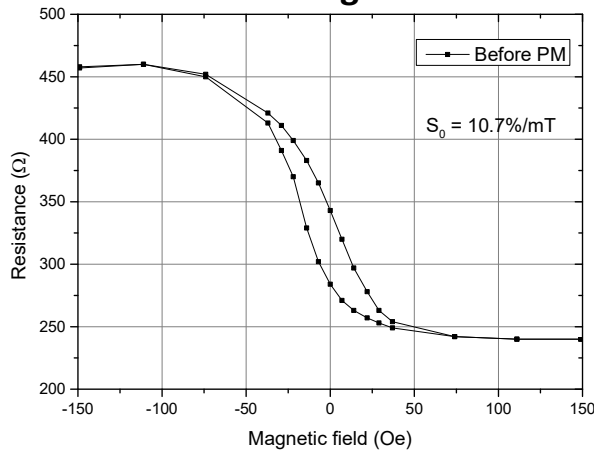
ferromagnetic material

→ Other toner/ink formulations also present ferromagnetic properties (e.g. MICR)

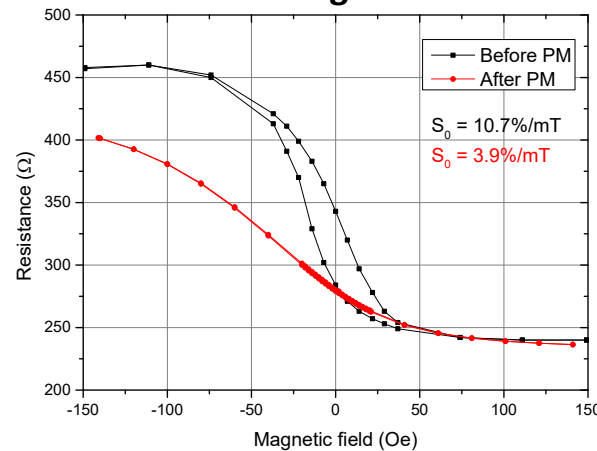
Alignment

Disc magnet provides a limited region where $B < 1 \text{ mT}$ ($\pm 170 \text{ } \mu\text{m}$) \rightarrow requires good accuracy from the alignment procedure

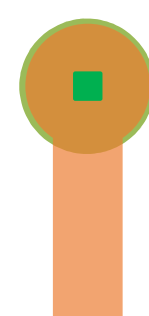
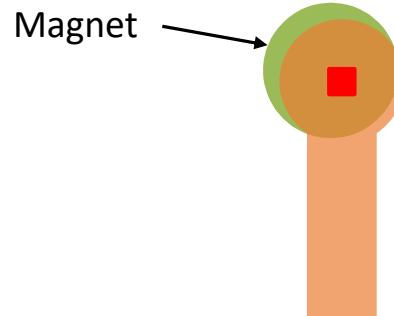
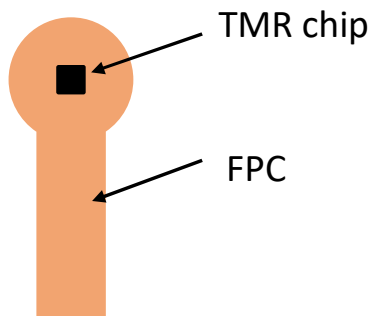
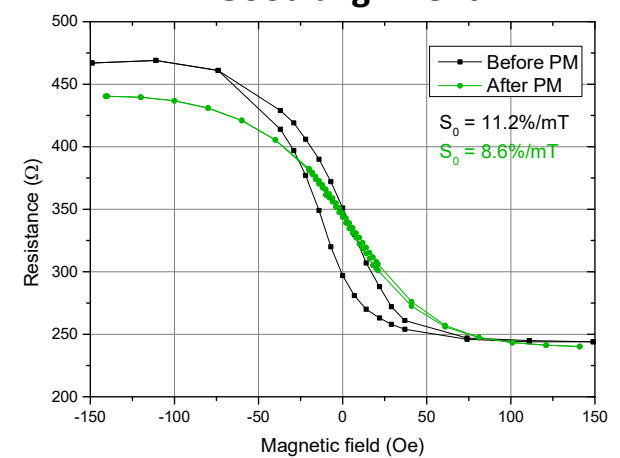
No magnet



Poor alignment

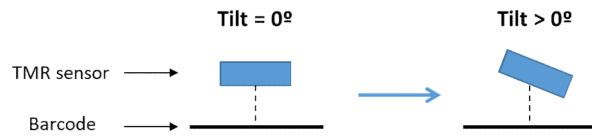


Good alignment



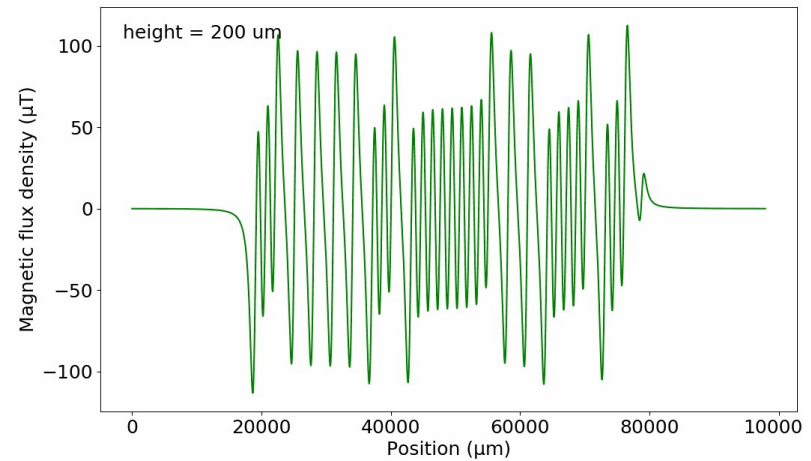
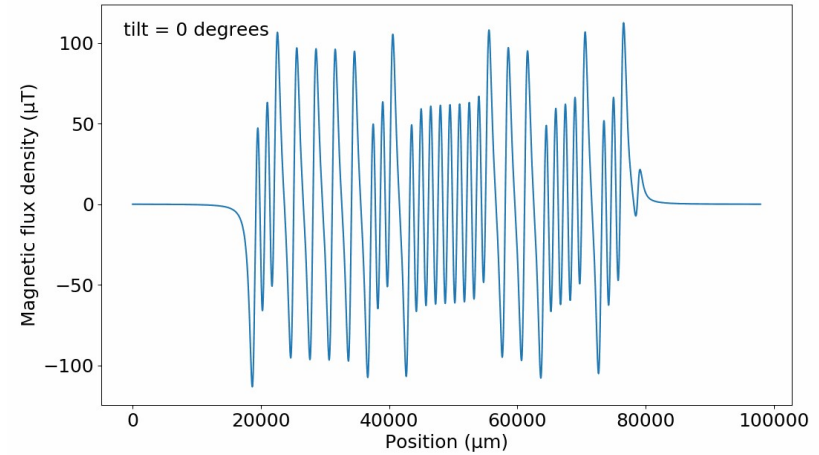
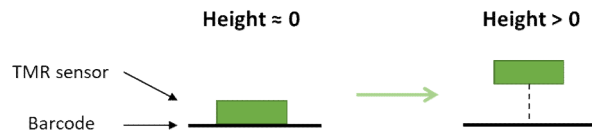
S.Abrunhosa, S.Cardoso, et.al
IEEE Trans. Magn. 58 (8), 4002304 (2022)

Swipe reader: assembly



Purpose:

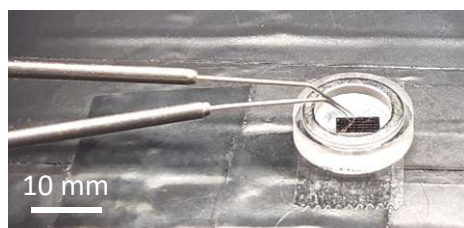
- Hold reader components
- Protect sensor chip
- Limit sensor tilt
- Minimise sensor-barcode distance



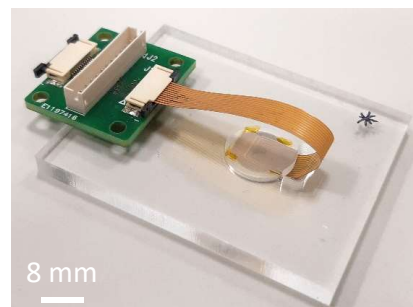
Handheld magnetic code reader



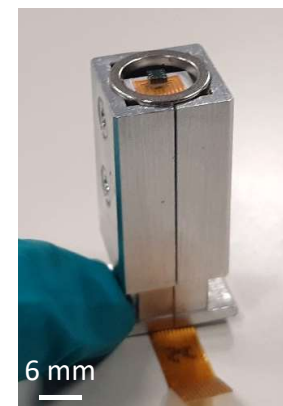
February 2020



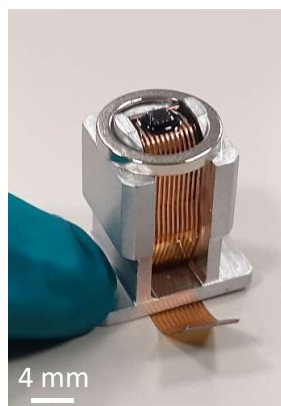
May 2020



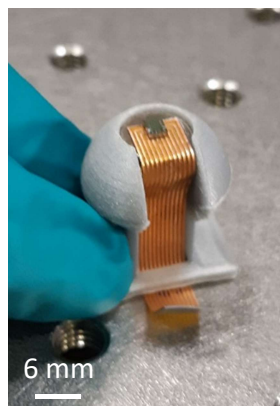
July 2020



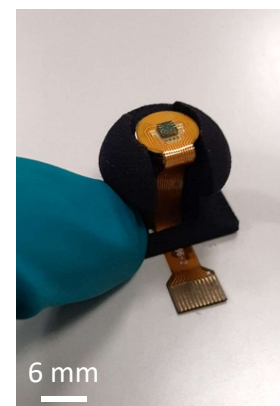
September 2020



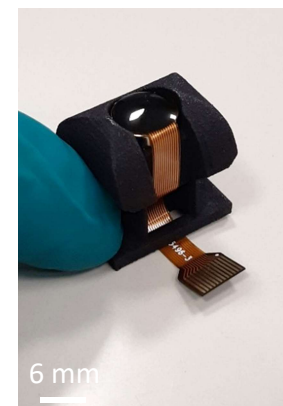
October 2020



December 2020

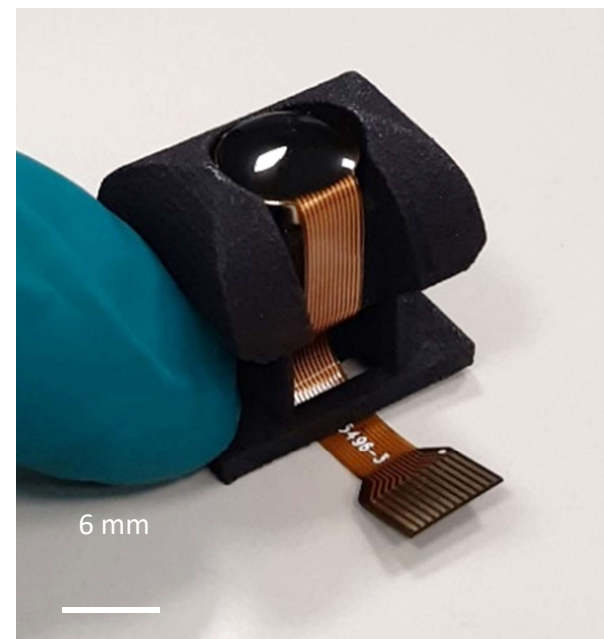
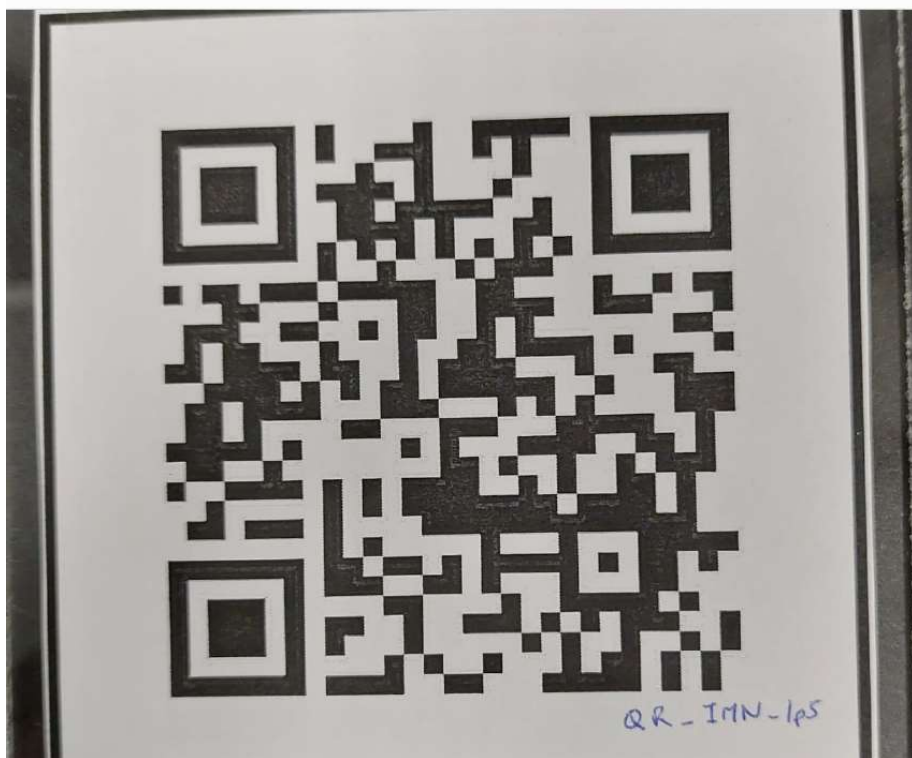


February 2021



...

Handheld magnetic code reader



NEXT CHALLENGE:
Decode QR codes

Acknowledgments

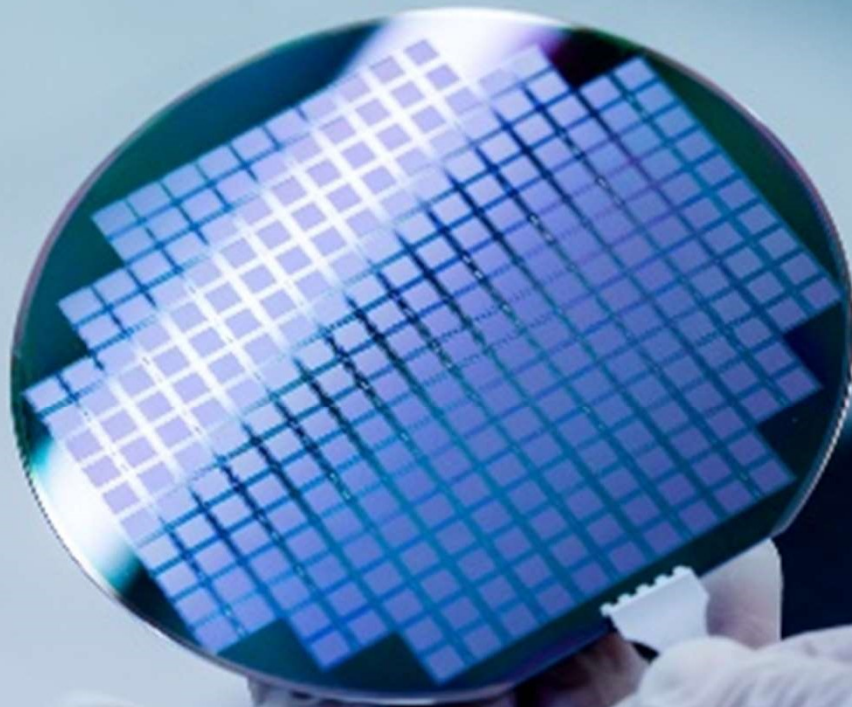
To my team at INESC-MN (past and present)



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scardoso@inesc-mn.pt



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